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# Silane/TiO<sub>2</sub> coating to control the corrosion rate of magnesium alloys in simulated body fluid

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# Highlights

- A well-developed silane/TiO<sub>2</sub> coating controlled corrosion rate of two Mg alloys.
- The protective ability of the coating depends upon the nature of the alloy.
- A Mg(OH)<sub>2</sub> and Ca/PO<sub>4</sub> containing layer of corrosion products was found.
- The coating favors the formation of a non-stoichiometric hydroxyapatiterich layer.

## **Abstract**

A silane-based coating modified with titanium IV iso-propoxide was developed to slow down the corrosion rate of AZ31 and ZE41 magnesium alloys intended as biodegradable implants materials. Electrochemical impedance spectroscopy (EIS) was used to monitor the corrosion evolution over 7 weeks in simulated body fluid at 37°C. A homogeneous crack-free 3µm-thick coating provided corrosion protection for 2 and 3 weeks to the ZE41 and the AZ31, respectively.

The corrosion mechanisms and the nature of the corrosion products of the coated systems are discussed and correlated to the coating morphology before and after the immersion tests.

Keywords: A. Magnesium; A. Alloy; B. EIS; C. Polymeric coatings; C. Alkaline corrosion.

#### 1. Introduction

Magnesium (Mg), and particularly its alloys, have drawn interest as biodegradable materials over the last years [1-4]. Compared to other biomaterials, Mg alloys present a considerable number of advantages: (i) high strength-to-weight ratio makes them suitable for load-bearing applications; (ii) their elastic modulus (~43 GPa) is close to that of bone minimizing stress shielding effect; (iii) Mg is present in large amount in the human body and it is essential for several metabolic processes [5-10]. However, the corrosion resistance of Mg alloys is poor and they undergo a rapid dissolution in simulated physiological media [11]. Indeed, this behaviour makes them unsuitable for fabrication of permanent implants such as endoprosthesis or hip replacement devices. However, it is possible to take advantage of their rapid biodegradation to design temporary implants. Particularly in bone repair therapy, Mg alloys have shown to be beneficial for bone growth and strengthening [12].

The rapid intrinsic degradation of Mg alloys in chloride-containing solutions, including human blood plasma [13], has hindered their widespread clinical application so far. In addition to the unfavourable corrosion kinetics of Mg, the accompanying hydrogen evolution ( $H_{evo}$ ) is a major issue. Hydrogen gas pockets adjacent to the implant can be formed causing structural disorders of the surrounding tissues and delay the healing process [14]. In addition,  $H_{evo}$  leads to local increase of the pH that might induce toxicity events [15]. Surface coating have shown to be a promising strategy to slow down the corrosion rate of Mg alloys and modulate it to levels at which detrimental effects are negligible [4]. Considering that these coatings must interact in a favourable manner with bone cells, many of the current approaches incorporate hydroxyapatite particles resulting in hybrid/composite layers [15-17]. Alternative options rely on the deposition of bioactive layers that favour hydroxyapatite precipitation from simulated body fluids (SBFs) [18, 19]. Those containing TiO<sub>2</sub>, a recognized biocompatible oxide, have high potential for surface functionalization of Mg alloys [20].

In the present study we propose a silane-based coating formulation, modified with titanium iso-propoxide to slow down and to control the corrosion rate of Mg alloys intended as biodegradable implants. The study was performed using electrochemical impedance spectroscopy in simulated body fluid (SBF) at physiological temperature. Depending upon the alloy system, the corrosion mechanisms are discussed.

#### 2. Experimental procedures

#### 2.1. Materials and substrate preparation

Extruded rods of AZ31 and ZE41 alloys (ASTM designation) with the chemical composition indicated in Table 1 (as detailed by the manufacturer Magnesium Elektron Company) were used in the present study. Discs of diameter 25 mm and 3mm-thick were grinded sequentially with 180, 400, and 1000 SiC grit papers and pre-treated with 12% HF solution by immersion for 15 minutes to promote the formation of a MgF<sub>2</sub> surface layer [21]. All discs were rinsed with ethanol (96%, Sigma-Aldrich) and dried in air stream as final step.

#### 2.2. Synthesis of the sol-gel coating and thermal conditioning

The coating formulation was selected based on previous investigations [22] and optimized for the purpose of this work. Two different alkolsols were mixed to obtain the final hybrid coating using the sol-gel route. The first alkolsol was prepared in the presence of acetylacetone (Acac, analytical standard) by the hydrolysis of 70% titanium (IV) isopropoxide (≥97% TIP, Aldrich) in iso-propanol. Diluted aqueous solution of HNO<sub>3</sub> (pH 0.5) was added resulting in a final volume ratio TIP:Acac:H<sub>2</sub>O of 5:3:1. The second silane-based alkolsol was obtained by the acidic hydrolysis (pH 0.5) of (3-glycidoxypropyl)trimethoxysilane (≥98% GPTMS, Aldrich) in iso-propanol and stirred for 1h at room temperature. The final volume ratio of GPTMS:2-propanol:H<sub>2</sub>O was 8:8:1. Finally, the titanium-containing and the silane-based alkolsols were mixed together in a volume ratio of 1:1.5, respectively. The combined solution was aged at room temperature for 1 hour and deposited onto AZ31 and ZE41 pre-treated discs by the dip-coating technique. The dipping parameters were 3 immersions of 10 seconds each at a withdrawal speed of 17 cm/min. The final step after dip-coating procedure was to dry the samples at 120°C for 90 minutes in air. Four conditions were tested: 12% HF pre-treated discs of the alloys designed as (i) AZ31 and (ii) ZE41; (iii) coated AZ31 alloy (AZ31\_S) and (iv) coated ZE41 alloy (ZE41\_S).

#### 2.3. Morphological characterization

or examining the morphology and chemical composition of the coating, field emission gun scanning electron microscope (FEG-SEM) JEOL-JSM7001F equipped with an energy dispersive spectroscopy (EDS) microanalysis was used. All the samples were coated with Au using a sputter coater system and examined before and after the immersion tests. Additionally, a diffracted backscattered electron detector (EBSD) appended to the SEM was used to assess crystallinity of the coating.

To determine the film thickness cross-sections were prepared by embedding the sample into an epoxy resin (Buehler) mould at room temperature and grinded up to 2500 SiC grit paper in ethanol.

A Nanosurf Easyscan 2 atomic force microscope (AFM) apparatus was used to determine the coating roughness and to obtain additional morphological information. Unfiltered images of topography, vibration amplitude and phase contrast were obtained in non-contact mode (tapping) at different positions and magnifications on the surface at room temperature using silicon probes.

#### 2.4. Electrochemical techniques and corrosion products characterization

Electrochemical impedance spectroscopy (EIS) measurements were carried out in order to characterize the corrosion performance of the coated alloys. The study was performed in naturally aerated simulated body fluid (SBF) pH 7.4 at  $37\pm1^{\circ}$ C for 7 weeks. The spectra were recorded at different immersion times using a Gamry Ref. 600 potentiostat at open circuit potential in the  $10^{5}$  Hz down to  $10^{-1}$  Hz frequency range. The SBF was prepared following the procedure described in [23] with the composition listed in the Table 2.

A conventional three-electrode electrochemical cell was used, consisting in the sample as working electrode with an exposed area of 3.1 cm<sup>2</sup>, a saturated calomel electrode (SCE) as reference and platinum coil as counter electrode. All the experiments were performed in a Faraday cage to avoid electromagnetic interferences. The fitting parameters were obtained by analysing the results with ZView3® software.

X-ray diffraction analyses of untested and tested discs were performed using Cu  $K_{\alpha}$  radiation in a Bruker D8 ADVANCE diffractometer operating at 40kV and 30mA. Raman spectra were acquired in a LabRAM HR800 Evolution Horiba, with a solid-state laser source operating at 532 nm with a 180° backscattered geometry, 600 lines/mm grating spectrograph and laser beam power of 20 mW.

#### 3. Results

#### 3.1 Surface morphology of uncoated and as-prepared coated alloys

The grinded discs were pre-treated for 15 minutes in 12% HF solution before coating. Fig. 1a and 1b depict the topographic AFM images of the layer formed on the pre-treated discs. Previous studies [2, 24] reported that acid treatment with hydrofluoric acid provides a MgF<sub>2</sub> layer on Mg alloys, decreasing corrosion rate in SBF solution [24]. The surfaces of the pre-treated alloys reveal MgF<sub>2</sub> crystal strings following the surface roughness (Fig. 1a–1b).

The morphology of the layer formed on AZ31 showed more compact structure when compared to the layer on ZE41, filling the cleavages between grinded scratches.

Fig. 1c and 1d depict AFM and SEM images of the coating, respectively. Irregular-shaped aggregates ranging from 1–10  $\mu$ m in diameter were found on the as-deposited coating. Their distribution over the surface was random with some crowded areas (Fig. 1c). EDX analysis of the aggregates (Fig. 1d) revealed that they consisted of Si and Ti oxides, most likely undissolved particles during the sol-gel preparation step. Topographical AFM images confirmed a smooth and rather homogeneous coating surface of small roughness  $R_q$  21.9  $\pm$  2.1 nm apart from the agglomerates. SEM images showed that the coating did not present relevant defects, such as micro-cracks or micro-pores. Additional analysis by electron backscattered diffraction (EBSD) did not reveal the Kikuchi patterns, suggesting that the coating and the aggregates had predominantly an amorphous structure. This is in accordance to the irregular shape of the agglomerates. The coating showed a homogeneous thickness of ~3.2  $\pm$  0.4  $\mu$ m irrespectively of the alloy (Fig. 1e).

#### 3.2 Electrochemical monitoring of the corrosion evolution

Following the characterization of the coated alloys, the corrosion behavior was studied by EIS at open circuit potential. The measurements were performed by immersing the samples in SBF (7.4 pH) solution at  $37 \pm 1^{\circ}$ C. Fig. 2 shows the open circuit potential (OCP) evolution of pre-treated and coated alloys. The OCPs of the pre-treated discs increased to more positive values during first 3 days and remained constant about -1.52 V until 2 weeks. Then, the OCPs showed minor fluctuations around this value remaining nearly constant until week  $7^{th}$ . The initial rise in OCP can be related to the formation of a layer of corrosion products with protective barrier properties.

The presence of the coating shifts the initial OCPs toward more positive values compared to the uncoated alloys. The OCP of AZ31\_S increased slowly during first 3 days whereas that OCP of ZE41\_S decreased. After 3 days, OCP of AZ31\_S slowly decreased due to degradation of the coating barrier properties. On the other hand, the OCP of ZE41\_S stabilized after 3 days followed by a small increase until week 3<sup>th</sup>. Then, the OCP showed a temporary increase to -1.46 V around 4 weeks. This feature was also reflected on the EIS results and will be discussed below along with characterization of the corrosion products.

Representative Bode plots obtained for the HF pre-treated alloys (AZ31 and ZE41) and the coated alloys (AZ31\_S and ZE41\_S) are depicted in Fig. 3 and Fig. 4, respectively. The low frequency impedance values of coated alloys at early immersion were two orders of

magnitude higher compared to the pre-treated samples, evidencing that the coating provides an effective barrier effect.

The initial low frequency impedance values of the coated alloys were similar, around 6  $\times 10^4 \,\Omega \cdot \text{cm}^2$  (see Fig. 4). However, with time relevant changes were observed. First, low frequency ( $10^{-1} \,\text{Hz}$ ) impedance of AZ31\_S showed minor fluctuations during first 72 hours. Next, impedance decreased being one order of magnitude lower around week 4<sup>th</sup>. At the same time, the high frequency time constant ( $10^3 - 10^5 \,\text{Hz}$ ) gradually vanished due to deterioration of the coating barrier properties.

In the case of ZE41\_S, impedance dropped during first 72 hours to a value almost one order of magnitude lower compared to AZ31\_S at the same immersion time. However, impedance of ZE41\_S revealed a significant increase at later stages. From  $2^{nd}$  to  $4^{th}$  week of immersion the low frequency impedance reached values of  $\sim 2 \times 10^5 \, \Omega \cdot \text{cm}^2$ . After this period, the impedance decreased once again to values of  $\sim 9 \times 10^3 \, \Omega \cdot \text{cm}^2$  after week  $7^{th}$ . Unlike AZ31\_S, the high frequency time constant of ZE41\_S was always detected in the spectra during the immersion period. In both coated alloys there were evident signs of corrosion activity. To further detail the nature and morphology of the corrosion products a detailed characterization was carried out.

#### 3.3 Morphology and composition of the corroded surfaces

Fig. 5 depicts the surface morphology of uncoated and coated discs after EIS experiments for 7 weeks. The cracks formed on the corrosion products layers, as observed in Fig. 5a–5b, may be due to volumetric contraction during dehydration process after electrolyte removal and the vacuum atmosphere during SEM analysis. Defects as cracks and local delamination evolved in the coating for both AZ31\_S and ZE41\_S (see Fig. 5c–5d). The arrow in Fig. 5d indicates a delaminated area with flake-like shape. These defects, as well as cracks, were randomly scattered over the entire surfaces. The morphology of the delaminated areas is likely due to local accumulation and growth of corrosion products at the substrate/coating interface as well as to hydrogen evolution (H<sub>evo</sub>). Visual inspection of the coated samples during immersion revealed the progressive formation of pits. In the ZE41\_S discs the first pits appeared after week 1<sup>st</sup>. In the case of AZ31\_S, identical pits appeared during week 3<sup>th</sup>.

EDX analysis of the pre-treated samples revealed the elemental composition of the corrosion products layers. The presence of Mg, O, Ca, P and C was detected (Table 3). The results evidenced the incorporation of Ca, P and C into the corrosion products. Nevertheless,

part of the carbon content may come from atmosphere impurities and part from surface deposits too. Calcium and phosphorus come from SBF solution.

To perform EDX analysis on the corrosion products of the coated discs the coating was manually removed. The corrosion layers of AZ31\_S and ZE41\_S contained higher amount Mg, O, Ca and Cl elements compared to the pre-treated discs. These results suggest that the local environment created by the presence of the coating along with the corrosion processes may promote the formation of P and Ca-enriched corrosion products. Additional XRD measurements confirmed that the corrosion layers consisted of Mg(OH)<sub>2</sub>. Broad diffraction peaks, as observed in Fig. 6a-6b, may suggest poor crystallinity of these layers. In the case of AZ31 the peaks of Mg(OH)<sub>2</sub> were not detected by XRD. There may be two possible explanations of this fact: (i) either the corrosion layer on AZ31 at 7 weeks is amorphous, (ii) or the layer is not thick enough to be detected by XRD. Fig. 7a shows a XRD pattern of pre-treated AZ31 after 1 week of immersion where the peaks corresponding to Mg(OH)<sub>2</sub> are clearly observable. This result suggests that crystallinity of the corrosion layers, particularly on AZ31, decreased with the immersion time. In aqueous solutions with high chloride concentrations Mg(OH)<sub>2</sub> reacts with Cl<sup>-</sup> to produce highly soluble MgCl<sub>2</sub> [25, 28]. According to this, one hypothesis may be that the former Mg(OH)<sub>2</sub> layer might become MgCl<sub>2</sub> and dissolve gradually into the solution. In Fig. 3a and 3b it is possible to see that setting-up of the corrosion layers on uncoated discs took place during first 3 days. This is in close agreement with the steep OCP rise for the same period of time as observed in Fig. 2.

Further Raman characterization supported the aforementioned hypothesis. Fig. 7b displays the Raman spectrum of the corrosion layer on AZ31\_S and ZE41\_S at week 7<sup>th</sup>. The peak at 3648 cm<sup>-1</sup> corresponding to the O-H fundamental of Mg(OH)<sub>2</sub> on the high frequency side was detected on both samples. Since Raman scattering is sensitive to the degree of crystallinity, broader peak and decreased intensity of AZ31\_S corrosion layer may indicate lower crystallinity when compared to the corrosion layer of ZE41\_S.

Further Raman results confirmed the presence of Ca and P in the corrosion layer of both coated discs, as reported in EDX results in Table 3. The corrosion layers consisted then in a mixture of Mg(OH)<sub>2</sub> and hydroxyapatite (HAP) for both AZ31\_S and ZE41\_S. The Fig. 8 depicts Raman spectra of coated discs in comparison to RRUFF<sup>TM</sup> patterns [29] of hydroxyapatite (Ref. 060180) and clorapatite (Ref. 060192). It has been reported in previous studies [30] that precipitation kinetics is critical for the purity of HAP and its crystallographic characteristics. Most of the synthetic methods to produce HAP crystals from supersaturated aqueous solutions led to the formation of non-stoichiometric products. This is due to the presence of vacancies and ion substitutes in the crystal lattice such as hydrogen phosphates,

carbonates, potassium and chlorides, among others [30]. Usually, these species are introduced into the precipitating system with the reactants. Hence, synthetized HAPs incorporating any of the above-mentioned ions undergo significant changes and have different crystal morphology compared to the stoichiometric [30]. This may explain the differences observed in the Raman spectra of AZ31\_S and ZE41\_S. Correspondingly, the Ca/P molar ratios listed in Table 3 suggest that in the present case the HAPs precipitated from SBF differ from stoichiometric HAP whose Ca/P molar ratio is 1.67. Other authors [27] have also reported that during immersion in SBF, the corrosion of Mg alloys is accompanied by the formation of corrosion products such as magnesium hydroxide, carbonates and phosphates. Cross-sectioning of coated samples revealed additional features of the corrosion layers. Fig. 9a shows the cross-section of AZ31\_S where a rather thin corrosion layer with a thickness in the range of 4–5 µm is observed. Nevertheless, the layer seems to have a dense structure. The local delamination of the coating due to accumulation of corrosion products is also seen in Fig. 9a. This corresponds to the flake-like shaped delaminated areas aforementioned and depicted in Fig. 5c-5d. The occurrence of localized corrosion (pits) was also observed on both AZ31\_S and ZE41\_S corrosion layers (not shown). The local environment created by the pit formation may promote the pile-up and growth of corrosion products around the pit. Apart from these areas, the thickness of the AZ31\_S corrosion layer seemed quite homogeneous.

In the case of ZE41\_S, a non-uniform corrosion layer of thickness ranging from 20 to 40 µm was observed (Fig. 9b). Large areas where the layer was detached possibly due to further corrosion were also found. Some of these areas reached about 90 µm in depth. This may explain the wide OCP variations of ZE41\_S as observed in Fig. 2. During first 3 days of immersion the OCP of ZE41\_S slightly dropped probably due to deterioration of the coating barrier properties. Next, the OCP stabilized and started rising slowly until week 3<sup>th</sup>. It appeared that the corrosion layer formation took place during this period of time. Then, thickening and densification of the layer could happen from week 3<sup>th</sup> to week 4<sup>th</sup>. However, the occurrence of pits in the corrosion layer enables the electrolyte to reach the metal surface and further corrosion causes selective detachment of the layer. The proposed corrosion mechanism would explain the OCP drop after 4 weeks of ZE41\_S and will be further discussed together with the parameters extracted from the EIS fitting.

#### 4. Discussion

#### 4.1 Corrosion mechanism and modelling

The most representative redox reactions responsible for the overall corrosion process of Mg alloys are listed below [22]:

Cathodic reactions	$2H_2O + 2e^- \rightarrow 2OH^- + H_2 \uparrow$	(Eq. 1)
	$O_2 + 2H_2O + 4e^- \rightarrow 4OH^-$	(Eq. 2)
Anodic reaction	$Mg \rightarrow Mg^{2+} + 2e^{-}$	(Eq. 3)
Overall reaction	$Mg + 2H_2O \rightarrow Mg(OH)_2 + H_2$	(Eq. 4)

As indicated by Eq. 4, the main products of the corrosion reaction are hydrogen gas and insoluble magnesium hydroxide. The local conditions may also promote the formation of hydroxides of the alloying elements and hydrated oxides [26].

The main role of the coating is to hinder water and oxygen access to the Mg substrate and especially to slow down the corrosion rate at early stages of immersion. This is possible due to the formation of stable Si-O-metal bonds which provide good adhesion to the substrate delaying corrosion onset [22]. The coating matrix is composed of a TiO<sub>2</sub>- and SiO<sub>2</sub>-containing network with good barrier properties that hinders electrolyte uptake and protects the underlying metal from accelerated corrosion [44]. However, in the present case the main objective of coating is to control the corrosion process and not to prevent it completely. Consequently, a thin coating was prepared allowing the electrolyte to gradually reach the metal substrate and the corrosion processes start. The corrosion activity leads to chemical and physical degradation of the coating due to initial swelling and subsequent setting-up of corrosion products. The local alkaline environment at the metal/coating interface promotes corrosion products growth inducing mechanical stresses to the coating which results in delamination and cracking. These defects further facilitate the electrolyte access to the alloy surface and the evolution of the corrosion processes.

Taking into account that the coating thickness and morphology was reproducible for both alloys, it can be suggested that the response of the coated discs over immersion reflects the respective corrosion susceptibility of the alloy. The impedance modulus of AZ31\_S showed a more stable behaviour when compared to that of ZE41\_S, as observed in Fig. 4. The low frequency impedance of ZE41\_S revealed a significant increase after 2 weeks suggesting the formation of a protective layer of corrosion products (see Fig. 4b). However, this protective effect was temporary and the impedance modulus decreased at a later stage. The ZE41 magnesium alloy contains rare-earth (RE) elements that may form protective RE oxides and hydroxides, decreasing the corrosion rate [43, 45]. Then, it is reasonable to think that the formation of the corrosion layer on ZE41\_S took place during first 2 weeks of immersion followed by densification from 2 to 4 weeks. After 4 weeks, nucleation and growth of defects

in the layer due to the presence of aggressive Cl<sup>-</sup> ions allowed further corrosion and consequently a decrease of the impedance values.

In contrasts, the initial corrosion rate of AZ31\_S was slower compared to ZE41\_S. There may be two complementary reasons of this fact: (i) at early immersion the corrosion resistance of AZ31 alloy in SBF is higher than that of ZE41 alloy and, (ii) the coating barrier properties degrade slower on AZ31 alloy. The first rationale may be supported by the impedance values of the uncoated samples plotted in Fig. 3. The second rationale may be explained by the middle-high frequency time constant that gradually vanished over immersion (Fig. 4a). Additionally, the corrosion layer formed on AZ31\_S seemed to have a quite dense and homogeneous structure (Fig. 9a). All the above mentioned, may be responsible for the rather stable behaviour of AZ31\_S during immersion.

To detail the EIS results numerical fitting of the experimental data was carried out using the equivalent circuit depicted in Fig. 10a. In this model, constant phase elements (CPE) representing non-ideal capacitors were considered instead of pure capacitors. Non-ideal capacitor behaviour may be due to factors such as electrode porosity, non-uniform current distribution and variations of the coating composition [3]. The physical interpretation of the equivalent circuit is also depicted in Fig. 10 and accounts for the presence of three time constants: (i) one at high frequencies describing the barrier properties of the coating; (ii) a second one in the medium frequency range assigned to interfacial corrosion layer and, (iii) a third one at low frequencies assigned to localized corrosion activity. The  $\chi^2$  of the regression was around  $10^{-3}$ .

In Fig. 10a CPE<sub>coat</sub> accounts for the capacitive response of the coating and CPE<sub>IL</sub> for the capacitive response of the interfacial layer (IL). It is important to note that at the beginning of the experiments the interfacial layer corresponds to the MgF<sub>2</sub> layer. However, with time this layer transforms into the corrosion products that build up underneath the coating. Likewise, R<sub>coat</sub> and R<sub>IL</sub> account for the resistance of the solution inside the narrow coating pores and the resistance of the pores in the IL, respectively.

Fig. 10b–10e depict the evolution of the different parameters extracted from the numerical fitting. The initial values of the pore resistance ( $R_{coat}$ ) for both coated alloys were similar. This is reasonable since at the beginning of the immersion the coating governs the corrosion response. In this case the as-deposited coatings had similar thickness and morphology on both alloys. The barrier properties of the coating can, thus, be characterized by  $R_{coat}$  and  $CPE_{coat}$ . When  $R_{coat}$  decreases and  $CPE_{coat}$  increases the coating barrier properties deteriorate and its protective ability decreases. In Fig. 10d the initial increase in Q for  $CPE_{coat}$  (0.66 < n < 0.89) of AZ31\_S may be attributed to electrolyte uptake, hereinafter the coating

barrier properties started to degenerate. From the behaviour of the Q parameter for CPE $_{\text{coat}}$  (0.1 < n < 0.81) of ZE41\_S it may be considered that the coating barrier properties deteriorate faster on ZE41 alloy. This is probably due to the increased corrosion activity of this alloy at early stages of immersion. Consequently, deposition and growth of the corrosion layer may occur at a faster rate inducing mechanical stresses to the coating matrix that result in structural defects, compromising the physical integrity of the coating at an earlier stage.

At the beginning of immersion R<sub>IL</sub> of AZ31\_S was higher compared to R<sub>IL</sub> of ZE41\_S. As depicted in Fig. 1a–1b, the MgF<sub>2</sub> layer on AZ31 alloy had a more compact structure when compared to the same layer on ZE41 alloy. As immersion elapses, the MgF<sub>2</sub> layer gradually dissolves and is replaced by the layer of corrosion products. Therefore, a more permeable MgF<sub>2</sub> layer along with higher corrosion susceptibility can lead to the fast drop in R<sub>IL</sub> of ZE41 S during first 24 hours.

The impedance of a CPE is given by the following equation [3]:

$$Z_{CPE}(\omega) = Q^{-1}(j \cdot \omega)^{-n}$$
 with  $-1 < n < 1$  (Eq. 5)

where j is the imaginary number and  $\omega$  is the angular frequency ( $\omega = 2\pi f$ , with f as the frequency). The Q parameter of CPE becomes equal to capacitance when n=1 and equal to resistance when n=0. An inductor corresponds to n=-1. The n values corresponding to CPE<sub>IL</sub> of AZ31\_S, indicated that the interfacial layer behaviour is closer to an ideal capacitor (0.88 < n < 0.95). This confirms that the Mg(OH)<sub>2</sub>/HAP layer (see Fig. 9a) formed on AZ31\_S was quite stable over immersion being responsible for the passive corrosion behaviour.

The charge transfer resistance ( $R_{ct}$ ) closely followed the  $R_{IL}$  variations. The Q values of the double layer capacitance ( $CPE_{dl}$ , 0.90 < n < 0.98) of AZ31\_S decreased from 24 hours to 1 week probably due to coating swelling. At this point the corrosion processes had already started. The precipitation/accumulation of corrosion products blocked the pores and defects in the coating through which the ions from the electrolyte are transported. The ions cannot reach the substrate and consequently the  $CPE_{dl}$  decreased. The subsequent decline of the coating barrier properties reactivates these pathways and corrosion processes can proceed.

The wide fluctuations in  $R_{\rm IL}$  and  $CPE_{\rm IL}$  (0.62 < n < 0.95) of ZE41\_S indicated that its corrosion layer structure varied over immersion (Fig. 10c and 10e). An increase in the  $R_{\rm IL}$  means that the IL structure becomes more compact [27]. In the same way, a decrease in the Q

parameter for CPE<sub>IL</sub> may be attributed to thickening of the layer. The capacitance of parallel plates is expressed by the following expression [27]:

$$C = \epsilon A / d \tag{Eq. 6}$$

where  $\epsilon$  is permittivity of the dielectric material between plates and A and d the area and separation of the parallel plates of the capacitor, respectively. Analogically, Q is equivalent to capacitive response (C) and d to the corrosion layer thickness. As observed in Fig. 10c and 10e, the initial increase in both R<sub>IL</sub> and Q for CPE<sub>IL</sub> of ZE41\_S suggest that the corrosion layer forms from 24 hours to week 1<sup>st</sup>. After 1 week, the continuous rise in R<sub>IL</sub> and the corresponding decrease in Q for CPE<sub>IL</sub> may indicate densification and thickening of the IL, respectively. As depicted in Fig. 9b, large areas of the Mg(OH)<sub>2</sub>/HAP layer on ZE41\_S were detached. These areas may expose either a new-fresh-metallic surface that reacts with the electrolyte to initiate the formation of a new fraction of the corrosion layer, or a cavitated zone in the corrosion layer that may become thicker afterwards. If this process is cyclic, it can be reflected in wide variations of the resistance and the capacitive response. Since resistance is inversely proportional to capacitance, the overall impedance response will be governed by the process with the highest Q value [33].

Lamaka et al. [22] studied the corrosion performance of ZK30 (3.0 wt% Zn, 0.3 wt% Zr) Mg alloy coated with a hybrid GPTMS:Ti coating doped with Ce<sup>3+</sup> ions. The study demonstrated that precipitation of Ce(OH)<sub>3</sub> and Ce(OH)<sub>4</sub> contributed to seal the corrosion layer structure, leading to a temporary increase of its resistance. Alkalinisation at the substrate/coating interface is likely to promote the formation of rare-earth hydroxides that may contribute to the initial stability of the ZE41\_S corrosion layer. The fact that these hydroxides were not detected by EDX analysis may be due to their lower content in comparison to other elements. In respect to x-ray diffraction results, the equipment used in this study may have low analytical limit and therefore patterns from precipitates in low quantity and crystal phases traces are difficult to detect. Moreover, Raman results suggested that the ILs of both AZ31\_S and ZE41\_S were poorly crystalline. Ascencio et al. [3] studied the influence of immersion time on the corrosion mechanisms of WE43 (4.0 wt% Y, 3.0 wt% RE) Mg alloy in modified SBF. They found that changes in the impedance response at advanced stages of immersion (120 hours) were due to rupture of the corrosion layer and lateral growth of stable pits [3]. Furthermore, from combined ART-FTIR and XRD results they demonstrated that the top-most corrosion layer was composed of an amorphous Mg(OH)<sub>2</sub> and carbonated apatite mixture [3].

The response of  $R_{ct}$  and Q for  $CPE_{dl}$  (0.76 < n < 0.98) of ZE41\_S showed that these parameters were governed initially by the coating properties, and thereafter by the formation and breakdown of the protective corrosion layer. After week 5<sup>th</sup>, the resistance and the capacitive response of ZE41\_S stabilized. This may be due to enlarged coating delaminated areas. When delaminated areas extent and reach a large fraction of the total coated surface, the corrosion becomes almost uniform and the electrochemical response is close to that expected for the uncoated metal.

The presence of Ca and P in the corrosion products layer revealed that the SBF influences the nature of the corrosion products, as reported by Ascencio et al. [3]. Li et al. [31] suggested that a Mg(OH)<sub>2</sub> layer provides favourable sites for hydroxyapatite nucleation via calcium immobilization on its surface. These nuclei grow spontaneously, consuming the calcium and phosphate ions from the surrounding fluid [32]. As pH rises, the ion strength of the electrolyte increases and hence the ionic activity inducing formation of Ca-P nuclei and their posterior growth. The formation of the nuclei induces changes in the barrier properties of the formed interfacial Mg(OH)<sub>2</sub> layer and can contribute for the observed impedance fluctuations too. Worth of notice is the fact that Ca and P were detected in higher quantities in the coated discs. This might be related to more concentrated local alkalinization in the buried areas where the coating delaminates.

Taken together, these data indicate that the coating can efficiently slow down the corrosion of the here studied Mg alloys in SBF under static conditions. However, further experiments would be required to extrapolate these results to the *in vivo* condition where the complexity of the biological fluids, the dynamic conditions as well as the mechanical loads acting over the materials can all together impact on their final corrosion behavior. Nevertheless, it must be pointed out that the deposition of a corrosion layer containing hydroxyapatite on the metal surface should favors bone deposition on the implant surface and consequently limit metallic ions accessibility into the body fluids. In this sense, this study contributes to the development of a route to control the corrosion activity of Mg alloys intended to be used as biodegradable metallic implants.

#### 4. Conclusions

Thin TiO<sub>2</sub>-modified silane coatings can be used to slowly control the corrosion rate of AZ31 and ZE41 Mg alloys. The coating barrier properties degrade faster on the rare-earth containing ZE41 alloy, due to its decreased corrosion resistance at early stages of immersion. However, the build-up of a thick Mg(OH)<sub>2</sub>/hydroxyapatite layer, as observed in the SEM analysis, induces wide variations on the corrosion activity as confirmed by electrochemical

impedance results. Contrarily, the Mg(OH)<sub>2</sub>/hydroxyapatite layer formed on the coated AZ31 alloy is thinner and shows a more stable behavior, degrading slowly over time.

In all the tested materials the results reveal the formation of calcium- and phosphateenriched corrosion products. However, the presence of the coating determines the composition of the calcium and phosphate compounds formed. The increase of the calcium to phosphate molar ratio in the coated discs can be assigned to a non-stoichiometric hydroxyapatite, as demonstrated by the Raman analysis. The presence of these compounds is an essential feature for the increased biocompatibility of these materials in bone repair applications.

#### Acknowledgements

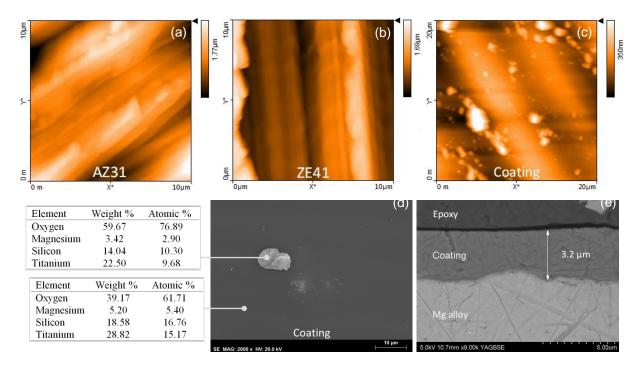
The authors acknowledge the financial support of the project 2012-05-EM from the International Doctoral School in Functional Materials IDS-FunMat and the financial support by Fundação para a Ciência e Tecnologia (FCT) to CQE (UID/QUI/00100/2013).

#### References

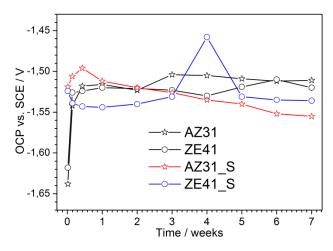
- [1] F. Witte, Acta Biomater. 6 (2010) 1680-1692.
- [2] M. Jamesh, S. Kumar, T.S.N. Sankara Narayanan, Corrosion Science 53 (2011) 645–654.
- [3] M. Ascencio, M. Pekguleryuz, S. Omanovic, Corrosion Science 87 (2014) 489–503.
- [4] W. Jin, G. Wu, H. Feng, W. Wang, X. Zhang, P.K. Chu, Corrosion Science 94 (2015) 142–155.
- [5] M.P. Staiger, A.M. Pietak, J. Huadmai, G. Dias, Biomaterials 27 (2006) 1728-1734.
- [6] H.S. Brar, M.O. Platt, M. Sarntinoramont, P.I. Martin, M.V. Manuel, JOM 61 (2009) 31-34.
- [7] Y. Yun, Z. Dong, N. Lee, Y. Liu, D. Xue, X. Guo, J. Kuhlmann, A. Doepke, H.B. Halsall, W. Heineman, S. Sundaramurthy, M.J. Schulz, Z. Jin, V. Shanov, D. Hurd, P. Nagy, W. Li, C. Fox, Mater. Today 12 (2009) 22-32.
- [8] X.-N. Gu, Y.-F. Zheng, Front. Mater. Sci. China 4 (2010) 111-115.
- [9] D. Persaud-Sharma, A. McGoron, J. Biomim. Biomater. Tissue Engin. 12 (2012) 25-39.
- [10] Y. Chen, Z. Xu, C. Smith, J. Sankar, Acta Biomater. 10 (2014) 4561-4573.
- [11] Renlong Xin, Yuanming Luo, Ailing Zuo, Jiacheng Gao, Qing Liu, Materials letters 72 (2012) 1-4.
- [12] T. Okuma, Magnesium and bone strength, Nutrition 17 (2001) 679-680.
- [13] V. Kaesel, P.-T. Tai, Fr.-W. Bach, H. Haferkamp, F. Witte, H. Windhagen, Approach to control the corrosion of magnesium by alloying, in: K.U. Kainer (Ed.), Proceedings of the Sixth International Conference Magnesium Alloys and Their Applications, 2003, pp. 534.
- [14] Guangling Song, Corrosion Science 49 (2007) 1696–1701.
- [15] M.F. Montemor, Surface & Coatings Technology 258 (2014) 17–37.
- [16] A. Zomorodian, M.P. Garcia, T. Moura e Silva, J.C.S Fernandes, M.H. Fernandes, M.F. Montemor, Acta Biomaterialia 9 (2013) 8660–8670.
- [17] A. Zomorodian, M.P. Garcia, T. Moura e Silva, J.C.S. Fernandes, M.H. Fernandes, M.F. Montemor, Materials Science and Engineering C 48 (2015) 434–443.
- [18] Anawati, Hidetaka Asoh, Sachiko Ono, Surface & Coating Technology 272 (2015) 182-189.
- [19] Fang Gao, Chenyang Xu, Huating Hu, Qi Wang, Yuanyang Gao, Hao Chen, Materials letters 138 (2015) 25-28.
- [20] J.Y. Han, Z.T. Yu, L. Zhou, Applied Surface Science 255 (2008) 455–458.

- [21] Sangeetha Kunjukunju, Abhijit Roy, Madhumati Ramanathan, Boeun Lee, Joe E.
- Candiello, Prashant N. Kumta, Acta biomaterialia 9 (2013) 8690-8703.
- [22] S.V. Lamaka, G. Knörnschild, D.V. Snihirova, M.G. Taryba, M.L. Zheludkevich, M.G.S. Ferreira, Electrochimica Acta 55 (2009) 131.
- [23] ISO/FDIS 23317:2007(E).
- [24] H. Bakhsheshi-Rad, M.H. Idris, M.R. Abdul-Kadir, M. Daroonparvar, Trans. Nonferrous Met. Soc. China 23(2013) 699–710.
- [25] R.C. Zeng, Y. Hu, S.K. Guan, H.Z. Cui, E.H. Han, Corrosion Science 86 (2014) 171–182.
- [26] H.E. Friedrich, B.L. Mordike. Magnesium Technology, Springer-Verlag, Berlin, Heidelberg, 2006.
- [27] X. Li, Z. Weng, W. Yuan, X. Luo, H.M. Wong, X. Liu, S. Wu, K.W.K. Yeung, Y. Zheng, P.K. Chu, Corrosion Science 102 (2016) 209–221.
- [28] Yanying Zhu, Guangming Wu, Yun-Hong Zhang, Qing Zhao, Applied Surface Science 257 (2011) 6129–6137.
- [29] Lafuente B, Downs R T, Yang H, Stone N (2015) The power of databases: the RRUFF project. In: Highlights in Mineralogical Crystallography, T Armbruster and R M Danisi, eds. Berlin, Germany, W. De Gruyter, pp 1-30.
- [30] S. Koutsopoulos, J Biomed Mater Res 62:600–612, 2002.
- [31] Zijian Li, Xunan Gu, Siquan Lou, Yufeng Zheng, Biomaterials 29 (2008) 1329–1344.
- [32] T. Kokubo, Thermochimica Acta 280/281 (1996) 479 490.
- [33] R. Pinto, M.G.S. Ferreira, M.J. Carmezim, M.F. Montermor, Electrochimica Acta 56 (2011) 1535-1545.
- [34] K.A. Yasakau, M.L. Zheludkevich, S.V. Lamaka, M.G.S. Ferreira, J. Phys. Chem. B 110 (2006) 5515.
- [35] J. Vormann, Mol. Aspects Med. 24 (2003) 27.
- [36] H. Zreiqat, C.R. Howlett, A. Zannettion, P. Evans, G. Schulze-Tanzil, C. Knabe, Biomed. Mater. Res. 62 (2002) 175.
- [37] Ren Y, Wang H, Huang J, Zhang B, Yang K, Eng Mater 2007;342–343:601–4.
- [38] Ren Y, Huang J, Zhang B, Yang K, Front Mater Sci Chin 2007;1:401–4.
- [39] Shaw BA, Wolfe RC, Corrosion of magnesium and magnesium-base alloys. In: Cramer
- SD, Convino BS, editors. ASM handbook, vol. 13B. Corrosion of materials. Metals Park, OH: ASM International; 2005. p. 205–27.
- [40] P. Córdoba-Torres, M. Keddam, R.P. Nogueira, Electrochim. Acta 54 (2008) 518.
- [41] N.T. Kirkland, N. Birbilis, M.P. Staiger, Acta Biomaterialia 8 (2012) 925-936.

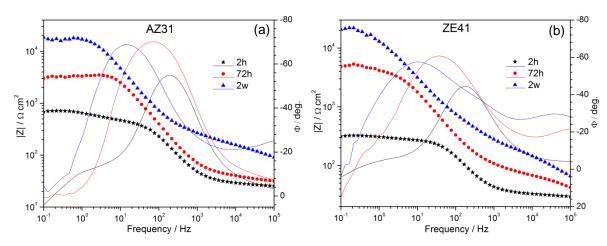
- [42] G. Baril, N. Pébère, Corros. Sci. 43 (2001) 471.
- [43] J. Meng, W. Sun, Z. Tian, X. Qiu, D. Zhang, Corr. Prevention of Magnesium Alloys (2013) 38-60.
- [44] S.K. Poznyak, M.L. Zheludkevich, D. Raps, F. Gammel, K.A. Yasakau, M.G.S. Ferreira, Progress in Organic Coatings 62 (2008) 226–235.
- [45] A. Ulrich, N. Ott, A. Tournier-Fillon, N. Homazava, P. Schmutz, Spectrochimica Acta Part B 66 (2011) 536–545.
- [46] R.C. Zeng, Y. Hu, S.K Guan, H.Z. Cui, E.H. Han, Corrosion Science 86 (2014) 171–182.
- [47] F. Rosalbino, E. Angeleni, S. de Negri, A. Saccone, S. Delfino. Intermetallics 13 (2005) 55.
- [48] Peixin Zhu, Yoshitake Masuda, Kunihito Koumoto, Biomaterials 25 (2004) 3915–3921.



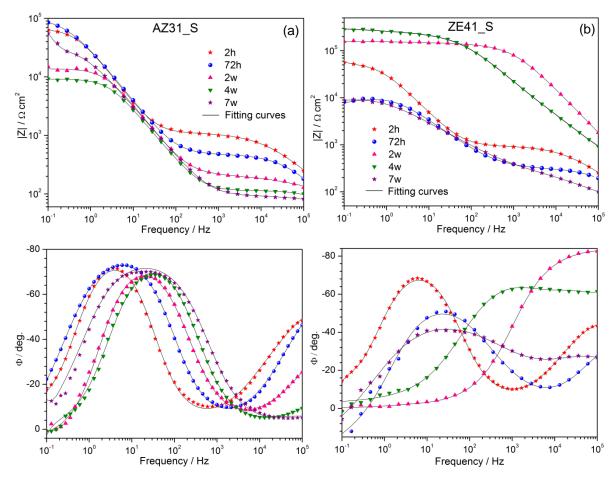
**Fig. 1.** Topographical AFM images of MgF<sub>2</sub> layer on (a) AZ31 and (b) ZE41, (c) as-deposited coating. Secondary electron image of (d) as-deposited coating with EDX results and (e) backscattered electron image of coating cross section.



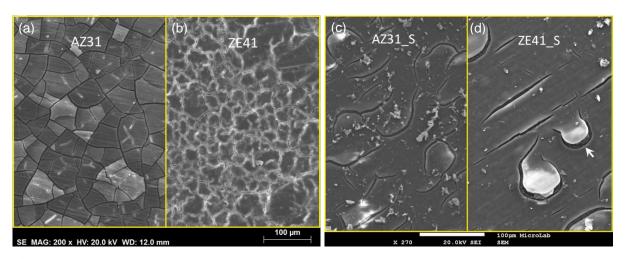
**Fig. 2.** OCP evolution of pre-treated and coated alloys in SBF (pH 7.4) at  $37\pm1$  °C.



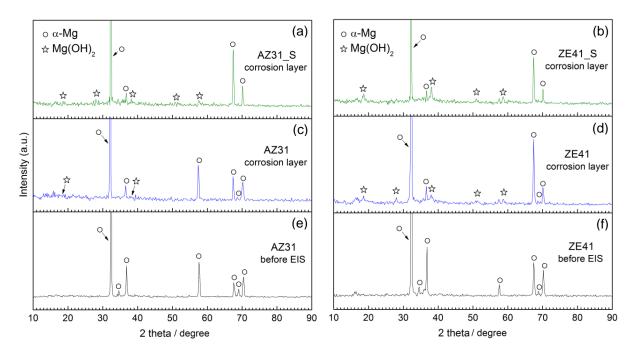
**Fig. 3.** Bode plots of pre-treated (a) AZ31 and (b) ZE41 immersed in SBF (pH 7.4) at  $37\pm1$  °C. Symbols are impedance values |Z| and lines are phase angle values ( $\phi$ ).



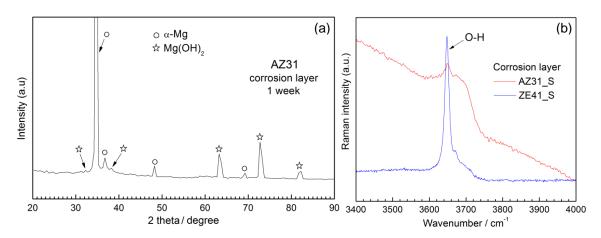
**Fig. 4.** Bode plots of coated (a) AZ31\_S and (b) ZE41\_S immersed in SBF (pH 7.4) at  $37\pm1$  °C for 7 weeks.



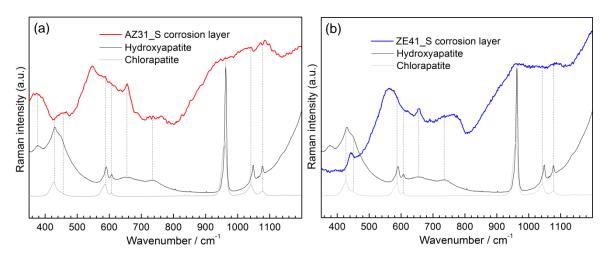
**Fig. 5.** Morphology of uncoated and coated discs after EIS experiments in SBF at 37±1°C for 7 weeks: (a) AZ31, (b) ZE41, (c) AZ31\_S and (d) ZE41\_S.



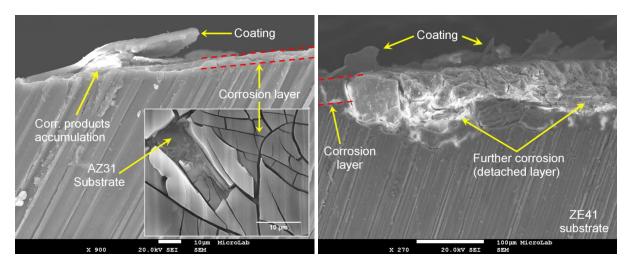
**Fig. 6.** XRD patterns of the corrosion layers on coated (a) AZ31\_S, (b) ZE41\_S and pretreated (c) AZ31, (d) ZE41. XRD patterns of pre-treated (e) AZ31 and (f) ZE41 before EIS.



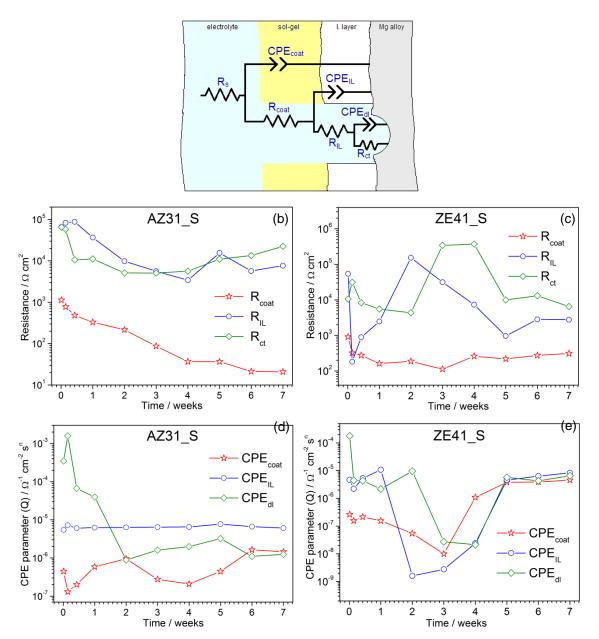
**Fig. 7.** (a) XRD pattern of corrosion layer on AZ31 after 1 week and (b) Raman spectra of the corrosion layers on AZ31\_S and ZE41\_S after 7 weeks in SBF at 37°C.



**Fig. 8.** Raman spectra of the corrosion layer on (a) AZ31\_S and (b) ZE41\_S after 7 weeks in comparison to hydroxyapatite and chlorapatite Raman spectra [29].



**Fig. 9.** Cross-sectional secondary electron images of (a) AZ31\_S and (b) ZE41\_S after 7 weeks in SBF at 37°C. The inset in (a) depicts a plane-view of the AZ31\_S corrosion layer after coating removal.



**Fig. 10.** (a) Equivalent circuit used to fit the EIS data. Evolution of the resistance for (a) AZ31\_S and (b) ZE41\_S. CPE parameter Q for (c) AZ31\_S and (d) ZE41\_S.

**Table 1.** Chemical composition of the Mg alloys.

Alloy	Al	Zn	RE*	Zr	Mn
AZ31	3	1	_	_	0.3
ZE41	_	4.3	1.3	0.6	_

<sup>\*</sup> Ce, La, Nd and other rare earths

**Table 2.** List of reagents required to prepare 1000 ml of SBF (pH 7.4).

Reagents <sup>a</sup>	g
NaCl	8.035
NaHCO <sub>3</sub>	0.355
KCl	0.255
$K_2HPO_4\cdot 3H_2O$	0.231
MgCl <sub>2</sub> ·6H <sub>2</sub> O	0.311
1M-HCl	40 (ml)
CaCl <sub>2</sub>	0.292
Na <sub>2</sub> SO <sub>4</sub> TRIS	0.072
(CH <sub>2</sub> OH) <sub>3</sub> CNH <sub>2</sub>	6.118
1M-HCl <sup>b</sup>	0–5 (ml)

<sup>&</sup>lt;sup>a</sup>Listed in sequence of

dissolution

<sup>&</sup>lt;sup>b</sup>To adjust pH 7.4

**Table 3.** Surface chemical composition of all tested conditions before and after EIS measured by EDX.

Elemental composition, atomic %									
Before EIS	О	Mg	Al	Before		O	Mg	Zn	
					EIS				
pre-treated	19.09	77.09	2.61	pro	pre-treated		80.62	2.71	
AZ31	17.07	11.07	2.01	ZE41		15.23	80.02	2./1	
Corrosion	О	Mg	Ca	P	С	Cl	Si	Ti	Ca/P
layer*									
AZ31	38.47	11.49	1.71	2.03	40.95	0.32	-	_	0.84
ZE41	45.08	16.22	1.74	2.26	33.58	0.73	_	_	0.77
AZ31_S	76.00	15.82	2.82	1.18	_	2.08	2.09	0.59	2.39
ZE41_S	71.99	17.08	3.01	1.47	_	2.21	2.56	1.89	2.04

<sup>\*</sup>After 7 weeks in SBF at 37±1°C