



**HAL**  
open science

## Ectopic expression of a mechanosensitive channel confers spatiotemporal resolution to ultrasound stimulations of neurons for visual restoration

Sara Cadoni, Charlie Demené, Ignacio Alcalá, Matthieu Provansal, Diep Nguyen, Dasha Nelidova, Guillaume Labernède, Jules Lubetzki, Ruben Goulet, Emma Burban, et al.

### ► To cite this version:

Sara Cadoni, Charlie Demené, Ignacio Alcalá, Matthieu Provansal, Diep Nguyen, et al.. Ectopic expression of a mechanosensitive channel confers spatiotemporal resolution to ultrasound stimulations of neurons for visual restoration. *Nature Nanotechnology*, 2023, 10.1038/s41565-023-01359-6 . hal-04067358

**HAL Id: hal-04067358**

**<https://hal.sorbonne-universite.fr/hal-04067358>**

Submitted on 13 Apr 2023

**HAL** is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

1 **Title:**

2

3 **Ectopic expression of a mechanosensitive channel confers spatiotemporal resolution to**  
4 **ultrasound stimulations of neurons for visual restoration**

5

6 **Author list:**

7 Sara Cadoni<sup>1</sup>, Charlie Demené<sup>2</sup>, Ignacio Alcalá<sup>1</sup>, Matthieu Provansal<sup>1</sup>, Diep Nguyen<sup>1</sup>, Dasha  
8 Nelidova<sup>3</sup>, Guillaume Labernede<sup>1</sup>, Jules Lubetzki<sup>1</sup>, Ruben Goulet<sup>1</sup>, Emma Burban<sup>1</sup>, Julie  
9 Dégardin<sup>1</sup>, Manuel Simonutti<sup>1</sup>, Gregory Gauvain<sup>1</sup>, Fabrice Arcizet<sup>1</sup>, Olivier Marre<sup>1</sup>, Deniz  
10 Dalkara<sup>1</sup>, Botond Roska<sup>3</sup>, José Alain Sahel<sup>1,4,5,6</sup>, Mickael Tanter<sup>2\*</sup>, Serge Picaud<sup>1\*</sup>

11

12 **Affiliation:**

13 <sup>1</sup>Sorbonne Université, INSERM, CNRS, Institut de la Vision, 17 rue Moreau, F-75012 Paris,  
14 France;

15 <sup>2</sup>Physics for Medicine Paris, INSERM, CNRS, École Supérieure de Physique et de Chimie  
16 Industrielles (ESPCI Paris), Paris Sciences et Lettes (PSL) Research University, 75012 Paris,  
17 France;

18 <sup>3</sup>Institute of Molecular and Clinical Ophthalmology Basel, Basel, Switzerland;

19 <sup>4</sup>Department of Ophthalmology, The University of Pittsburgh School of Medicine, Pittsburgh,  
20 PA 15213, United States;

21 <sup>5</sup>Department of Ophthalmology and Vitreo-Retinal Diseases, Fondation Ophtalmologique  
22 Rothschild, F-75019 Paris, France;

23 <sup>6</sup>Centre Hospitalier National d'Ophtalmologie des XV-XX, F-75012 Paris.

24 \*These authors contributed equally to this work.

25

26 Corresponding author: Serge Picaud (serge.picaud@inserm.fr)

27 <http://www.researcherid.com/rid/H-4012-2014>

28

29

30

31

32 **Abstract**

33 Remote and precisely controlled activation of the brain is a fundamental challenge in the  
34 development of brain-machine interfaces (BMI) for neurological treatments. Low-frequency  
35 ultrasound stimulation can be used to modulate neuronal activity deep in the brain especially  
36 after expressing ultrasound-sensitive proteins. But so far, no study has described an  
37 ultrasound-mediated activation strategy whose spatiotemporal resolution and acoustic  
38 intensity are compatible with the mandatory needs of BMIs, in particular for visual restoration.  
39 Here we combined the expression of large-conductance mechanosensitive ion channels  
40 (MscL) with uncustomary high-frequency ultrasonic stimulation to activate retinal or cortical  
41 neurons over millisecond durations at a spatiotemporal resolution and acoustic energy  
42 deposit compatible with vision restoration. The *in vivo* sonogenetic activation of the visual  
43 cortex generated a behaviour associated to light perception. Our findings demonstrate that  
44 sonogenetics can deliver millisecond pattern presentations via an approach less invasive than  
45 current BMIs for visual restoration.

46

47

48

49 **Main text**

50 **Introduction**

51 Brain-machine interfaces (BMIs) based on multi-electrode arrays have met with  
52 increasing success in peripheral sensory system rehabilitation strategies, for restoring hearing  
53 in the cochlea or sight in the retina<sup>1, 2</sup>. The restoration of vision is the most demanding  
54 challenge for BMIs, as it ultimately requires the 13Hz rate transmission of complex spatial  
55 patterns<sup>3</sup>. Although form perception can be achieved by epicortical or intracortical implants<sup>4</sup>,  
56 <sup>5</sup>, lack of long-term sustainability has intensified the search for non-contact distant activation  
57 of neuronal circuits. Optogenetic therapy has provided an alternative, as demonstrated on the  
58 retina even at the clinical level<sup>6</sup>. Despite encouraging animal studies<sup>7-9</sup>, approaches for optical  
59 stimulation of the cortex are hindered by the dura mater and by brain scattering and  
60 absorption of light requiring invasive light guides<sup>10</sup>.

61 Ultrasound (US) waves could potentially overcome these limitations to achieve the non-  
62 contact neuromodulation of cortical and subcortical areas of the brains<sup>11-17</sup>. However, this

63 neuromodulation requires a craniotomy (Fig 1.a) and the use of high US frequencies to  
64 reach the required spatial resolution. Switching from 0.5 MHz to 15 MHz would theoretically  
65 lead to a 30-fold improvement in resolution (Fig. 1c-e) and a ~27000-fold improvement in  
66 neuromodulated volume. Unfortunately, most existing US neuromodulation strategies are  
67 restricted to low-frequency<sup>15</sup> or mid-range<sup>18</sup> transmissions resulting in poor spatial resolution  
68 (>3 mm) and/or long lasting responses while 30 MHz high frequency was reported to generate  
69 inhibitory neuromodulation<sup>19</sup>. Other attempts at high-frequency neuromodulation have  
70 resulted in high levels of acoustic energy<sup>20</sup>, with risks of thermal heating<sup>21</sup> and tissue  
71 damage<sup>14</sup>.

72 Sonogenetic therapy has proposed to generate a neuronal mechano-sensitivity by  
73 ectopic expression of US-sensitive proteins like TRP1 ion channel<sup>22</sup>, mechanosensitive ion  
74 channel of large conductance (MscL)<sup>23</sup>, or auditory-sensing protein prestin<sup>24</sup> using AAV gene  
75 delivery to target specific cell populations<sup>23, 25, 26</sup> nevertheless without spatiotemporal  
76 resolution compatible for vision restoration. A high temporal resolution was shown for MscL  
77 only in primary cultured hippocampal neurons with mutations enhancing its pressure  
78 sensitivity<sup>27, 28</sup>, the MscL-G22S mutant boosting US sensitivity of *in vivo* neurons<sup>23</sup>.

79

80

81

82 We have here investigated if we can use the MscL channel<sup>29</sup> 1) to boost the neuronal  
83 sensitivity to US not only *ex vivo* but also *in vivo* , 2) to target a locally defined subset of  
84 neurons by gene therapy, 3) to induce responses with a temporal precision (millisecond time  
85 delay and recovery) sufficient for visual restoration and 4) to gain more than one order of  
86 magnitude in spatial resolution through the *in vivo* use of high-frequency US at low acoustic  
87 intensities to prevent adverse effects<sup>20</sup>.

88

### 89 **Sonogenetic activation on the *ex vivo* retina**

90 Using the retina as an easily accessible part of the central nervous system, we targeted  
91 MscL specifically into rat retinal ganglion cells (RGCs), with *in vivo* intravitreal delivery by an  
92 adeno-associated vector (AAV) encoding the *mscL* gene from *Escherichia coli* in its wild-type  
93 (WT) form or with the G22S mutation<sup>28</sup>. An AAV2.7m8<sup>30</sup> serotype vector was used to encode  
94 MscL fused to the red fluorescent protein tdTomato, under control of the SNCG promoter to  
95 target the RGC population<sup>31</sup>. On the eye fundus, tdTomato fluorescence was detected *in vivo*  
96 (Fig. 2a). Its expression was restricted to RGCs, as indicated by their double labeling with a  
97 specific RGC antibody, RPBMS (Figs 2b, E1b). Expression of the MscL channel seemed to be  
98 concentrated at the cell membrane on the soma and axon (Figs 2c, E1) with 24% and 46% of  
99 RPBMS-positive cells expressing tdTomato, for the MscL-WT and MscL-G22S proteins,  
100 respectively (Fig. 2d).

101 During *ex vivo* recordings of the MscL-expressing retina (Fig. 2e), RGCs displayed strong  
102 and sustained ON spiking responses to focused 15 MHz US stimulation (Fig. 2f- left)  
103 irrespectively of their ON or OFF responses to light (Fig. E2a). Many RGCs presented responses  
104 with very short latencies,  $12.2 \pm 2.5$  ms, (Fig. 2f- left), but some had longer latencies (Fig. 2g).  
105 By contrast, non-transfected (NT) retina displayed only long latency responses,  $50.4 \pm 4.2$  ms  
106 (Figs 2f-right, 2g). Synaptic blockers (CNQX-LAP4-CPP) abolished US responses in non-  
107 transfected retinas but not in MscL-transfected retinas, in which they decreased the number  
108 of long latency US responses (LL: latency of more than 45 ms, Fig. 2l, Fig E2c-d). This  
109 observation suggests that responses in non-transfected retina originate upstream from RGCs,  
110 as previously reported<sup>41</sup>. This conclusion was supported by the absence of US response in the  
111 retinas of non-transfected blind P23H rats having lost photoreceptors whereas transfected  
112 P23H showed a majority of short latency (SL) responses (<45ms) (Fig. 2l, Fig E2c-d). The

113 geometric mean latencies in MscL-tested groups were very different from those for the non-  
114 transfected retina especially in the blind p23H retina (Fig. E2c), but the cumulative distribution  
115 of latencies further highlighted these differences (Fig. E2d). These results suggested a natural  
116 mechanosensitivity in photoreceptors highly reminiscent to that of auditory cells in agreement  
117 with the expression of Usher proteins in both sensory cells. These Usher proteins are known  
118 for generating the auditory mechanotransduction and likely the phototropism of  
119 photoreceptors underlying the Stiles Crawford effect<sup>32</sup>.

120 MscL expression decreased latency and increased the mean number of cells per retina  
121 responding to US (Fig. 2h). Short latency (SL) responding cells expressing MscL were sensitive  
122 at much lower US pressures than non-transfected cells and their number increased with  
123 increasing US pressures (Fig. 2i). SL US responses also involved higher firing rates and were  
124 more sustained than LL US responses (Fig. 2j). Moreover, we observed that the G22S mutation  
125 further enhanced the sensitivity of SL RGCs to lower US pressures (Fig. 2k, E1b). We  
126 subsequently restricted our analyses to SL US responses (<45ms). Neurons responded to even  
127 very short stimulation durations (10 ms), with responses showing a fast return to the control  
128 level of activity (Fig. 3a). US response durations were correlated with stimulus duration  
129 although a reduction of the firing rate occurred for long stimuli (>100 ms) (Fig. 3c-d). Using  
130 different stimulus repetition rates, RGCs were able to follow rhythms up to a 10 Hz frequency  
131 (Fig. 3b-e). The Fano factor indicated that the response had a low variability in spike count and  
132 possibly high information content (Fig. 3c-e).

133 We then investigated whether different US frequencies (0.5, 2.25 and 15 MHz) affected  
134 the spatial resolution of the response, in accordance with the measured US pressure fields  
135 (Fig. E3). Transducers were designed with a similar focal distance and numerical aperture, for  
136 the transmission of focused beams over different frequency ranges (0.5, 2.25, 15 MHz,  
137 corresponding to wavelengths of 3.0, 0.7 and 0.1 mm, respectively) (Fig. 1c-e). Features of the  
138 responses evoked by the different US frequencies were found to be similar (Fig. E2e-f)  
139 although increasing the frequency from 0.5 MHz (typical of neuromodulation) (Fig. 1c) to 15  
140 MHz (Fig. 1e) reduced the focal spot by a factor  $\sim 4100$  with our transducers. Cells responding  
141 to US were widespread over the recorded area for 0.5 and 2.25 MHz, but appeared to be more  
142 confined for 15 MHz (Fig. 3f), despite similar acoustic parameters (100ms: 1.1 and 1.3 MPa)  
143 for the 2.25 MHz and 15 MHz beams. The acoustic pressure at 0.5 MHz was lower (0.5 MPa)  
144 due to electric power limitation of our electronics. The spatial dispersion of activated cells

145 decreased significantly from  $1.48 \pm 0.12$  mm and  $1.30 \pm 0.18$  mm at 0.5 MHz and 2.25 MHz,  
146 respectively, to  $0.59 \pm 0.03$  mm at 15 MHz (Fig. 3g). This spatial dispersion was consistent with  
147 the size of the measured ultrasound pressure fields (Fig. 1c-e); for the 0.5 MHz transducer, the  
148 focal spot was much larger than the MEA chip. The density of activated cells increased  
149 significantly with increasing US frequency but on a smaller area (Fig. 3h). US stimulation is  
150 more effective at higher frequencies, because lower acoustic power values are required to  
151 activate an equivalent number of cells. Indeed, even if the acoustic intensities at 2.25 and 15  
152 MHz were quite similar, the acoustic power delivered was almost two orders of magnitude  
153 lower at 15 MHz (0.03 W) than at 2.25 MHz (0.82 W). At 15 MHz, moving the focal spot of the  
154 US probe above the retina triggered a shift in the area of responding cells (Fig. 3i). The  
155 response center was found to move in accordance with the displacement of the US transducer  
156 (Fig. 3j). These results demonstrate that our sonogenetic therapy approach can efficiently  
157 activate neurons with a millisecond and sub-millimetric precision.

158

#### 159 **Spatiotemporal resolution *in vivo* on the visual cortex**

160 We investigated whether the approach could also be applied to the brain *in vivo*  
161 through a cranial window (Fig. 1a,b). As the G22S mutation enhanced the US sensitivity of  
162 RGCs *ex vivo*, we expressed MscL-G22S in cortical neurons of the primary visual cortex (V1) in  
163 rats. We injected AAV9.7m8 encoding the MscL-G22S channel fused to tdTomato under the  
164 control of the neuron-specific CamKII promoter into V1. TdTomato fluorescence was detected  
165 in the brain (Fig. 4a) and in cortical slices, particularly in layer 4 (Fig. 4b). Staining with an anti-  
166 NeuN antibody showed that 33.4% of cortical neurons in the transfected area expressed  
167 tdTomato (Fig. 4c).

168 To measure responses to 15MHz US Stimulations, we placed a micro-EcoG ( $\mu$ EcoG)  
169 electrode array on the cortical surface of V1 (Fig. 4d). In non-transfected (NT) animals, no US-  
170 evoked signal was recorded (Fig. 4e-right,  $n=3$  rats), whereas, in V1 expressing MscL-G22S, US  
171 stimulation of the cortical surface elicited large negative  $\mu$ EcoG potentials (Fig. 4e-middle,  $n=6$   
172 rats). These US-evoked negative deflections were different from the recorded visual-evoked  
173 potentials (Fig. 4e-left). Amplitudes and durations of the US responses were clearly related to  
174 the duration of US stimulations (Fig. 4f, 4h) and US pressures (Fig. 4g). V1 cortical responses  
175 were again able to follow a repetition rate of up to 13 Hz (Fig. 4i) even if peak amplitude  
176 decreased slightly for increasing stimulation frequencies.

177           The peak depolarization of each channel was measured and linearly interpolated to  
178 build pseudocolor activation maps showing sizes of the US-responding cortical area  
179 dependent on the US pressure from 0.26 MPa ( $0.58 \pm 0.17 \text{ mm}^2$   $n=6$  rats) to 1.27 MPa ( $1.41 \pm$   
180  $0.23 \text{ mm}^2$   $n=5$  rats) (Fig. 4j-l). When the ultrasound probe was moved laterally, the source of  
181 the generated neuronal activity moved in a similar direction (Fig. 4k). The spatial location of  
182 the evoked potentials moved by 0.29 mm ( $\pm 0.09$  mm,  $n=6$  rats) from the previous location  
183 (Fig. 4m, Fig. E5), even though we moved the US transducer in 0.4 mm steps. This discrepancy  
184 between the displacement of the activated area and movement of the transducer was  
185 certainly related to the 0.3 mm discrete spatial pitch distribution of the electrodes and the  
186 lateral spread of activity in the circuit. These results suggest that our approach to sonogenetic  
187 therapy could yield a spatial resolution of within 400  $\mu\text{m}$  for stimulations at 15 MHz, the focal  
188 spot of our 15 MHz transducer being 276  $\mu\text{m}$  wide (Fig. 1d). This opens up the possibility of  
189 targeting small areas (down to  $0.58 \text{ mm}^2$  for 0.26 MPa), depending on the pressure level.  
190 These very localized US-evoked responses, their dependence on the position of the US probe  
191 and their short latencies confirmed that they were due to the activation of MscL-G22S-  
192 expressing neurons and not to an indirect response related to auditory activation, as  
193 previously suggested by others<sup>33, 34</sup>.

194           When recording with penetrating electrode arrays (Fig. 4d), V1 neurons expressing  
195 MscL-G22S generated sustained responses even to 10 ms-long 15MHz US stimuli (Fig. 5a) with  
196 latencies shorter than 10ms ( $5.10 \pm 0.62$  ms  $n=27$  cells) (Fig. 5b), consistent with a direct US  
197 activation. Responding neurons were recorded at various cortical depths, ranging from 100  
198  $\mu\text{m}$  to 1 mm (Fig. 5c), the focal spot diameter of the US probe being 3.75 mm in the xz plane.  
199 Deep neurons responded reliably to stimuli of decreasing duration, from 50 ms to 10 ms, with  
200 similar firing rates, whereas longer stimuli induced responses in a broader population of  
201 neurons (Fig. 5d-e). To investigate if an US pattern could be applied for visual restoration at a  
202 refreshing rate of up to 13 Hz, we increased progressively the sequence of stimuli. Cortical  
203 neurons were able to generate distinct responses to each US stimulus up to a 13 Hz repetition  
204 rate (Fig. 5f), but the number of responding cells decreased with increasing stimulus frequency  
205 (Fig. 5g). No major tissue temperature increase is expected even at this stimulation rate (Fig.  
206 E4).

207

208



## 209 Behavioral response to the sonogenetic stimulation of the visual cortex

210 To define if US-elicited synchronous activation of MscL-expressing excitatory cortical  
211 neurons can induce light perception, we assessed mouse behaviour during an associative  
212 learning test including 15 MHz US stimulation of V1 in MscL G22S-transfected ( $n=14$ ) and non-  
213 transfected ( $n=9$ ) animals (Fig. 6 and E6). Mice subjected to water deprivation were trained to  
214 associate the visible-light stimulation of one eye with a water reward (Fig. 6a)<sup>35</sup>. This task was  
215 learned within four days, as indicated by the increasing success rate during this period, from  
216  $30.9 \pm 17.9\%$  (SD) to  $86.2 \pm 14.1\%$  (SD) for MscL-G22S-transfected mice (Fig. 6b). The success  
217 rate was determined by assessing the occurrence of an anticipatory lick between the light  
218 onset and the release of the water reward 500 ms later (Fig. 6a). Only mice reaching a 60%  
219 success rate on the 4<sup>th</sup> day were retained for this analysis and sessions showing a compulsive  
220 licking rate were excluded. Following cortical US stimulation on day 5, MscL-G22S-transfected  
221 mice achieved a success rate  $69.3 \pm 25.4\%$  (SD), the difference of which showed no statistical  
222 difference with the success rate following light stimulation on day 4 (Fig. 6b). After a pause  
223 during the weekend (day 6-7), the animals retained the task, their success rates showing no  
224 statistically significant differences with the one following light stimulation (Fig. 6b). By  
225 contrast, in non-transfected animals, the success rate following the US stimulation of their  
226 visual cortex dropped to  $38.1 \pm 18.5\%$  (SD), the difference with the success rate following light  
227 stimulation on the 4<sup>th</sup> day was highly significant ( $p<0.0001$ ) (Figs 6d, E6). In the AAV-injected  
228 mice, we found that the latency of the first anticipatory lick was shorter for sonogenetic  
229 stimulation ( $187.1 \pm 37.3$  ms;  $n=14$ , SD) than for stimulation with a light flash ( $265.9 \pm 46.5$  ms;  
230  $n=23$ , SD) (Fig. 6c, E6d). This shorter latency for the US response is consistent with the faster  
231 activation of cortical neurons for sonogenetic stimulation than for light stimulation of the eye  
232 (Fig. 4e). In transfected mice, success rates increased with pressure (Fig. 6d), suggesting a  
233 brighter and/or a larger US-elicited percept with a greater US pressure as described with  
234 increasing currents in human patients<sup>4</sup>. Interestingly, the licking frequency during the 500 ms  
235 before delivery of the water reward also increased with US pressure (Fig. 6e). These results  
236 suggest that the sonogenetic stimulation of the visual cortex generates a perception in mice  
237 that is likely associated to a visual perception although more complex visual behaviors as form  
238 discrimination would be required for a demonstration.

239

240

241 **Safety issues**

242 Our sonogenetic approach greatly decreased the US pressure required for the  
243 activation of RGCs and V1 cortical neurons with stimulation sequences remaining below FDA  
244 safety limits (510k, Track 3) for US imaging (e.g. for a 10 ms US stimulus of 0.6 MPa, the non-  
245 derated  $I_{sptp}$  is 12 W/cm<sup>2</sup> and the non derated  $I_{spta}$  value is 0.12 W/cm<sup>2</sup>). These very low  
246 acoustic pressures and acoustic intensities prevent tissue damage, as they are similar to those  
247 that have been widely used in clinical diagnostic imaging for decades<sup>36</sup>. Moreover, simulations  
248 of US-induced heating in brain tissue revealed that typical US parameters (i.e. 20 ms, 1.27  
249 MPa) (Fig. 4e-h) increased the local temperature by an estimated 0.12 °C, with even high  
250 repetition rates (up to 13 Hz) leading to a moderate temperature increase (<0.3 °C) (Fig. E4c-  
251 f). These low-temperature fluctuations (corresponding to “worst-case” scenarios as we used  
252 non derated US parameters) and stimulation sequences compliant with FDA limits suggest  
253 that our approach had no toxic side effects and that US-elicited responses were not  
254 temperature-driven and were therefore probably mediated by mechanical activation of MscL  
255 channels by US. The fact that acoustics intensities and pressure used here remained far below  
256 the FDA requirements for conventional ultrasonic imaging in clinics  
257 (<https://www.fda.gov/media/71100/download>) and generated very low temperature  
258 increase in comparison with thermal damaging effects<sup>37</sup>, raises high hopes for a smooth  
259 clinical translation. Moreover, a very recent safety study by Cheng et al<sup>19</sup> demonstrated an  
260 absence of brain tissue damages using high frequency activation at ten times higher acoustic  
261 intensities (continuous insonication at 11.8 W/cm<sup>2</sup> compared to our “worst case”  $I_{spta}$  1.56  
262 W/cm<sup>2</sup> for repeated stimulations at 13 Hz rate).

263

264 **Conclusions**

265 The development of remotely controlled cortical and subcortical deep neuronal  
266 stimulation techniques is of considerable interest for the treatment of diverse neurological  
267 diseases and sensory handicaps. Most previous sonogenetic studies focused on the use of low-  
268 frequency US<sup>22-24</sup> as in the recent demonstration of MscL-based sonogenetic activation in  
269 mouse brain<sup>23</sup>. However, such low-frequency US waves lead to limited centimetric spatial  
270 resolutions (~5x5x45 mm<sup>3</sup>) and an uncontrolled spatial beam distribution. An alternative  
271 approach to spatially containing US stimulations involves the use of higher US frequencies, but  
272 this was thought to demand higher energy levels, exceeding safety limits and favoring tissue

273 damage<sup>20</sup>. The bacterial MscL channel has been reported to sensitize neurons to US<sup>23, 27, 28</sup> and  
274 to lower the pressure for neuronal activation, but its use for high-spatiotemporal resolution  
275 sonogenetic stimulation has yet to be shown to be effective *in vivo*. We here showed that  
276 that US activation of MscL-G22S expressed in retinal or cortical neurons resulted in responses  
277 with millisecond latencies and a spatial resolution of at least 400  $\mu\text{m}$  in the *xy* plane at a 15  
278 MHz frequency. The subsequent neuronal activation throughout the depth of the visual cortex  
279 (Fig. 5n-p) led to a behavioral motor response, suggesting light perception by the animal.  
280 These sonogenetic responses were genuinely related to MscL expression, as they were not  
281 observed in non-transfected animals. Following previous demonstrations that the MscL  
282 channel is a suitable sonogenetic actuator<sup>23, 27, 28</sup>, we provide further evidence that the MscL  
283 channel has appropriate kinetics for the activation of neurons at a precise spatiotemporal  
284 resolution *in situ* and *in vivo*.

285         The temporal precision of sonogenetics is lower than that achieved with optogenetic  
286 (> 40Hz) by the fastest opsins<sup>38</sup> and ChrimsonR<sup>39</sup>, which is successfully restoring vision at the  
287 retinal level in patients<sup>6</sup>. MscL only follows a 13 HZ frequency *in vivo*, which is in the same  
288 range as the 5-20 Hz achieved *in vivo* by the very sensitive opsin, ChRmine<sup>40</sup>, a frequency range  
289 likely sufficient for vision<sup>3</sup>. The discovery of ChRmine has enabled investigators to stimulate  
290 deep into the rodent brain even from above the skull<sup>40</sup>. Future studies will have to examine  
291 the spatial resolution of this approach and how it compares to sonogenetics. As for all gene  
292 therapies in non-dividing cells, both optogenetic and sonogenetic therapies are expected to  
293 be life long lasting as indicated by gene therapy in congenital Leber amaurosis although it did  
294 not stop the ongoing degeneration of photoreceptors in patients<sup>41</sup>.

295         Restoration of form vision at cortical level was previously achieved with 0.5 to 1 mm  
296 surface electrodes spaced more than 1 mm apart<sup>5</sup> or with 1.5-mm-long penetrating electrodes  
297 spaced 400  $\mu\text{m}$  apart<sup>4</sup>. The spatial resolution of the proposed sonogenetic therapy therefore  
298 appears to be compatible with the cortical restoration of form vision but with a remote non-  
299 contact device. To preserve this spatiotemporal resolution, the ultrasound stimulator will  
300 require to be placed directly above the dura mater or above an ultrasound transparent  
301 artificial skull<sup>42</sup>. At 15 MHz, the typical penetration depth with negligible heating is typically  
302 20 mm. Moreover, the resolution of the approach could be increased by using gene therapy  
303 to drive expression in specific cell populations and cell compartments<sup>31, 43</sup>. Further studies are  
304 required to generate an interface for coding visual information into US patterns transmitted

305 by an ultrasonic matrix array onto the visual cortex at a video rate. To reduce the ultrasound  
306 load, visual restoration can take advantage of event-based camera, heat-sensitive camera or  
307 depth filtering imaging to limit the active pixel number in an image<sup>44-46</sup>. Therefore, our  
308 approach provides great hope for the development of high-resolution visual restoration at the  
309 cortical level, through its unique combination of a rapid response, high spatial resolution, and  
310 cell selectivity with promoters. Even if this approach requires craniotomy, as for other existing  
311 visual prostheses, it provides a less invasive approach based on deep and distant cortical  
312 activation from above the dura mater following AAV cortical injections. More generally, it  
313 paves the way for a new type of genetic-based brain-machine interface capable of  
314 compensating for disabilities and suitable for use in treatments of neurological disorders.

### 315 **Acknowledgements**

316 The authors would like to thank C. Joffrois, M. Valet, Q. Cesar, M. Desrosiers, S. Fouquet, P.  
317 Annic, M. Celik, Z. Raics for technical help and scientific advice. This work was supported by  
318 the European Research Council (ERC) Synergy Grant Scheme (holistic evaluation of light and  
319 multiwave applications to high-resolution imaging in ophthalmic translational research  
320 revisiting the Helmholtzian synergies, ERC Grant Agreement #610110), by the European  
321 Union's Horizon 2020 research and innovation programme under grant agreement No.  
322 785219 (Graphene Flagship Core 2) No. 881603 (Graphene flagship Core3), by the Foundation  
323 Fighting Blindness, La Fondation pour la Recherche Médicale (FRM EQUIPE  
324 EQU202106012159), l'UNIM, *la Fédération des Aveugles de France*, Optic 2000, the city of  
325 Paris, *Région ile de France*, the *Agence Nationale de la Recherche* (ANR BrainOptoSight), and  
326 French state funds managed by the *Agence Nationale de la Recherche* (ANR) within  
327 *Programme Investissements d'Avenir, Laboratoire d'Excellence* (LABEX) LIFESENSES (ANR-10-  
328 LABX-0065) and *Institut Hospitalo-Universitaire* FOReSIGHT (ANR-18-IAHU-0001), by NIH  
329 CORE Grant P30 EY08098 to the Department of Ophthalmology, the Eye and Ear Foundation  
330 of Pittsburgh, and from an unrestricted grant from Research to Prevent Blindness, New York,  
331 NY.

332

### 333 **Author Contributions Statement**

334 S.C., C.D. designed the experiments. I.A., M.P. contributed equally. S.C., M.P., G.L., I.A., J.L,

335 R.G., E.B., J.D. carried out the experiments and analyzed the data, M.P., D.N., G.G., F.A., O.M.,  
336 D.D., M.S., B.R. provided support for experiments, study design and data analysis, S.P., M.T.,  
337 J.S. conceived the idea for this project and supervised the analysis of the data obtained. S.C.,  
338 C.D, I.A., M.T., S.P. wrote the manuscript. S.P. and M.T. contributed equally. All authors  
339 provided critical feedback on the research and the manuscript.

340

#### 341 **Competing interests Statement**

342 The authors have filed for a patent for devices and methods for sonogenetic stimulation.

343

344 **Tables:** None

345

#### 346 **Figure Legends/Captions**

347 **Fig. 1 Sonogenetics using focused ultrasound beams for visual restoration through the intact dura**  
348 **mater: impact of ultrasonic transmission frequency.** (a) Concept of visual restoration with US matrix  
349 arrays implanted in a cranial window for localized US neuromodulation of the primary visual cortex in  
350 humans. The US beam can be adaptively focused at different locations in the V1 cortex while passing  
351 through the intact dura mater, subdural and subarachnoid spaces. (b) Proof-of-concept setup used in  
352 this study for V1 sonogenetic activation in rodents, using a high-frequency focused transducer on a  
353 craniotomized mouse. (c) Characterization of the radiated field for the 0.5 MHz transducer used in this  
354 study. (top) Longitudinal view of the maximal pressure for a monochromatic acoustic field radiated at  
355 0.5 MHz by the 25.4 mm  $\emptyset$ , 31.75 mm focus transducer. Pressure maximum is reached at 25.9 mm,  
356 slightly closer to the transducer than the geometric focal point, which is a documented effect <sup>66</sup>.  
357 (middle) Transverse section of the maximal pressure field at depth  $z = 25.9$  mm. (bottom) One-  
358 dimensional profile of this transverse section giving the FWHM of the focal spot (4.36 mm at 0.5 MHz).  
359 (d) Same characterization for the 2.25 MHz 12.7mm  $\emptyset$  25.4 mm focus transducer. (e) Same  
360 characterization for the 15 MHz 12.7mm  $\emptyset$  25.4 mm focus transducer. Note that the maximum  
361 pressure is reached very close to the geometric focus (25.21 mm versus 25.4 mm for the geometric  
362 focus) for this configuration. The FWHM of the focal spot is 0.276 mm. Figures 1a and 1e were created  
363 with Biorender.com.

364

365

366 **Fig. 2 Sonogenetic therapy in rat retinal ganglion cells.** (a) *In vivo* retinal fundus image showing MscL-  
367 tdTomato expression. (b-c) Confocal stack projections across the retinal ganglion cell (RGC) layer of a  
368 flat-mounted retina. (d) Density of RBPMS-, MscL-positive and double-labeled cells ( $n=5$  MscL WT and  
369 G22s retinas, \*,  $p=0.0140$ , for RBPMS(+); \*,  $p=0.0465$ , for RBPMS(+)/MscL(+), unpaired two-tailed  $t$   
370 test). (e) Schematic diagram of the experimental setup with an image of the retina on MEA electrodes.  
371 (f) Representative peristimulus time histograms (PSTHs) for US or visual stimuli in MscL-transfected or  
372 non-transfected (NT) RGCs (US stimuli: 15 MHz, 1.27 MPa). (g) RGC response latencies to a 15 MHz US  
373 stimulus for MscL ( $n=300$  cells, 9 retinas) and NT retinas ( $n=41$  cells, 4 retinas). Dotted line: 45 ms  
374 latency threshold. (h) Number of cells per retina responding to 15 MHz US stimuli (0.98-1.27 MPa) for  
375 MscL ( $n=9$  retinas) and NT ( $n=4$  retinas) with short (< 45 ms, SL) or long latencies (> 45 ms, LL). \*  
376  $p=0.0002$ , unpaired two-tailed  $t$  test. (i) Mean number of SL-responding RGCs per retina following  
377 stimulation with US stimuli of increasing pressure for MscL ( $n=9$ ) and NT ( $n=4$ ) retinas. \*\*\*  $p=0.00008$ ,  
378 \*\*\*  $p=0.0010$ , \*\*\*  $p=0.0008$ , multiple unpaired two-tailed  $t$  test. (j) Maximum firing rate and response  
379 duration (of SL and LL RGCs from MscL retinas in response to US stimuli of increasing pressure (0.2-  
380 1.27 MPa) ( $n=9$  retinas, \*\*  $p=0.0017$ , \*  $p=0.0418$ , unpaired two-tailed  $t$  test). (k) Percentage of SL RGC  
381 cells (normalized against the maximum number of responsive cells in each experiment) responding to  
382 US stimuli for MscL WT ( $n=3$  retinas) and MscL G22S ( $n=6$  retinas) retinas. \*\*  $p=0.0065$ , \*\*  $p=0.0083$ ,  
383 multiple unpaired two-tailed  $t$  test. (l) Ratios of RGCs responding to US stimulation with short (SL) or  
384 Long latencies (LL) for MscL and NT retinas ( $n=9$  retinas for MscL and 4 for NT), following the application  
385 of a cocktail of synaptic blockers (CNQX-CPP-LAP4,  $n=3$  retinas for both MscL and NT), and for P23H  
386 retinas with and without MscL expression (both  $n=3$  retinas). \* Conditions with no US-elicited cell  
387 responses. Data are presented as mean values +/- SEM. Scale bars represent 100, 20, 200 $\mu$ m in b,c,e.

388

389

390

391

392 **Fig. 3 Spatiotemporal properties of sonogenetic retinal responses.** (a-b) Spike density functions (SDFs)  
393 of two RGCs from a MscL retina for 15 MHz stimulus durations and repetition frequencies (a: 0.5 Hz  
394 repetition rate, b: 10, 20, 50, 200 ms durations). (c) Maximum firing rates for different 15 MHz stimulus  
395 durations and mean Fano factor values for all cells (10-20 ms  $n=8$  retinas, 50-200 ms  $n=9$  retinas). (d)  
396 Correlation between response duration and stimulus duration ( $n=9$  retinas). (e) Maximum firing rates  
397 for different stimulus repetition frequencies and mean Fano factor values for all cells (0.2-2 Hz  $n=9$   
398 retinas, 5-10 Hz  $n=8$  retinas). (f) (Top) Retinas on a MEA chip and corresponding size of the incident US  
399 pressure beam (circles represent the FWHM and are centered on the estimated center of response),  
400 for 0.5, 2.25 and 15 MHz. (Bottom) Corresponding activation maps representing the normalized firing  
401 rates of the cells following US stimulation. Each square box represents an electrode with at least one  
402 US-activated cell. (g) Spatial dispersion of activated cells and (h) ratio of the number of activated cells  
403 to the stimulated area for the three US frequencies, \*\*\*\*,  $p=0.00002$  for panel g,  $p=0.00006$  (15 vs  
404 2.25 MHz) and  $p=0.00005$  (15 vs 0.5 MHz) for panel h, \*\*  $p=0.0008$ , \*  $p=0.0169$ , unpaired two-tailed  $t$   
405 test.  $N=12$  retinas for 0.5 MHz (0.29-0.68 MPa),  $n=5$  retinas for 2.25 MHz (1.11-1.62 MPa),  $n=9$  retinas  
406 for 15 MHz (1.12-1.27 MPa). (i) Heatmaps showing activated cells in a MscL retina following  
407 displacements (0.4 and 0.8 mm) of the US transducer. Circles represent the estimated center of the  
408 response. (j) Relative displacement of the center of the response following displacement of the 15 MHz  
409 US transducer. \*\*\*\*  $p=0.00001$ , \*\*  $p=0.0018$ , unpaired two-tailed  $t$  test.  $n=9$ , 9, and 6 positions for 4,  
410 4 and 2 retinas for displacements of 0,  $0.4 \pm 0.20$  and  $0.8 \pm 0.18$  mm (SD), respectively. The dotted gray  
411 line represents the theoretical displacement. Data are presented as mean values  $\pm$  SEM. Scale bars  
412 represent 1 mm in f (top) and 0.5mm in f (bottom) and i.

413

414

415

416 **Fig. 4 Spatial resolution of *in vivo* sonogenetic therapy in V1 cortical neurons.** (a) Image of a rat brain  
417 expressing MscL-G22S-tdTomato (red) in V1. (b) Confocal stack projection of a sagittal brain slice  
418 expressing MscL G22s-tdTomato (red) and labeled with anti-NeuN antibody (green) and DAPI (blue).  
419 The layers of V1 are delineated by dashed white lines. (Lower right) Magnification of layer 4 of V1. (c)  
420 Density of NeuN-positive, MscL-positive and double-labeled cells for 3 brain slices. (d) Schematic  
421 diagram of the setup used for *in vivo* electrophysiological recordings and US stimulation; (Top right)  
422  $\mu$ EcoG electrode array placed on V1 of a MscL-transfected rat. (e) (Left) Visual-evoked cortical  
423 potentials in response to a 100 ms flash. (Middle) Sonogenetic evoked potentials for 15 MHz US stimuli  
424 of various durations. (Right) Absence of US responses on a non-transfected (NT) rat to a 15 MHz  
425 stimulus. Black traces represent the mean evoked potential over 100 trials, individually illustrated by  
426 the gray traces. The black arrow indicates the stimulus onset. (f) Duration of sonogenetic  $\mu$ EcoG  
427 responses for stimuli of different durations (10 ms  $n=58$ , 20 ms  $n=32$  and 50 ms  $n=56$  trials on 6  
428 animals). (g) N1 peak amplitude for increasing US pressure, (h) increasing duration and (i) frequency  
429 ( $n=6$  rats). (j) Pseudocolor activation maps for stimuli of increasing US pressure and (k) for a horizontal  
430 displacement of the US transducer by 0.8 mm (the arrow indicates the direction of the displacement).  
431 Each black dot represents an electrode of the array. The color bar represents N1 peak amplitude in  $\mu$ V.  
432 (l) Mean activated area for various US pressure values ( $n=6$  animals). (m) Relative displacement of the  
433 activation center to the previous position following movement of the US transducer by 0.4 mm.  $p=1$   
434  $10^{-12}$ , one-sample two-tailed  $t$  test,  $n=37$  positions on 6 animals (Mean:  $0.29 \pm 0.16$  mm, SD). Data are  
435 presented as mean values  $\pm$  SEM. Scale bars represent 200 and 50  $\mu$ m in b, 300  $\mu$ m in j-k.

436  
437  
438



439 **Fig. 5: Temporal resolution of *in vivo* sonogenetic cortical activation.** (a) Spike density functions (SDF)  
440 of 58 and 27 neurons recorded with a penetrating multielectrode array in MscL-transfected rats  
441 following US stimulation for 50 and 10 ms. (Red: mean trace, grey: individual cells) (b) Response  
442 latencies following 50 and 10 ms US stimuli (50 ms  $n=58$  cells, mean:  $7.5 \pm 7.6$  ms (SD), 7 rats; 10  
443 ms  $n=27$  cells, mean:  $5.1 \pm 3.2$  ms (SD), 5 rats). (c) Depth of US-responding cells ( $n=58$ ) in MscL-  
444 expressing rats ( $n=7$ ). (d) Instantaneous SDF of responses to US stimuli of different durations (1 Hz  
445 stimulus repetition frequency). (e) Maximum firing rates ( $n= 27, 22, 58$  cells, SD: 55.8, 56.2, 49.8 ms  
446 for 10, 20 and 50 ms stimulation respectively) and numbers of activated neurons upon US stimulations  
447 of different durations (US pressure: 1 MPa). (f) Instantaneous SDF of responses to US stimuli of  
448 different repetition frequencies (10 ms stimulus duration). (g) Mean maximum firing rate and number  
449 of activated neurons upon US stimulation at different stimulus repetition frequencies (10 ms, 1MPa,  
450  $n= 27, 40, 30, 10, 13$  cells, SD: 55.8, 50.8, 55.7, 41.5, 58.2 Hz). Data are presented as mean values +/-  
451 SEM.

452

453

454

455

456

457

458 **Fig. 6 Behavioural response induced by sonogenetic activation of the V1 cortex in mice following**  
459 **associative visual training.** (a) Schematic diagram of the behavioral task performed by mice. Water-  
460 restricted animals trained in an associative learning paradigm for light stimulation (LS) with a water  
461 reward are subjected to either a light stimulation of the eye (day 1-4) or a US stimulation of V1 at 15  
462 MHz (day 5 and 8-10). (b) Mean rates of successful trials for 4 days of training during learning of the  
463 association between light stimulation (LS, green, 50 ms) and water reward followed by the US  
464 stimulation (US orange, 1.2 MPa) for MscL-G22S transfected mice (between Day 4 LS and Day 5 US: 50  
465 ms 1.2 MPa, ns  $p=0.0570$ . Between Day 5 US and Day 8 US: 50 ms 1.2 MPa, ns  $p=0.6079$ , two-tailed  
466 unpaired  $t$  test, Mean: 30.9, 49.9, 77.6, 86.2, 69.3, 62.3, 66.9, 76.5, SD: 17.9, 31.2, 13.9, 14.1, 25.4,  
467 35.4, 37.1, 27.7%,  $n=14$  animals) (c) Mean time to first lick after light (50 ms) and US stimulation (50  
468 ms, 1.2 MPa) (\*\*\*\*  $p=0.0000290$ , two-tailed unpaired  $t$  test,  $n=23$  and  $n=14$  animals, Mean: 265.9,  
469 187.1, SD: 46.5, 37.3 ms for LS and US respectively). (d) Mean rate of successful trials over 4 days of  
470 US stimulation for non-transfected (NT) and MscL-G22S transfected mice, following 50 ms of US  
471 stimulation at increasing US pressure (ns  $p=0.9452$ , \*\*\*  $p=0.0003$ , \*\*\*\*  $p=0.0000296$ , two-tailed  
472 unpaired  $t$  test, for 0.2, 0.7 and 1.2 MPa, respectively,  $n=14$  animals, Mean: 35.2, 60.8, 68.7, SD: 17.5,  
473 24.4, 23.6% for MscL-G22S;  $n=9$  animals, Mean: 35.7, 27.5, 27.8, SD: 12.4, 11.0, 13.2% for NT). (e)  
474 Session anticipatory lick rates for NT and MscL-G22S transfected mice at increasing US pressures (ns  
475  $p=0.6934$ , \*  $p=0.0119$ , \*\*\*\*  $p=0.0000340$ , two-tailed unpaired  $t$  test, for 0.2, 0.7 and 1.2 MPa,  
476 respectively,  $n=14$  animals, Mean: 1.4, 3.0, 4.1, SD: 0.4, 1.7, 1.8 Hz for MscL-G22S and  $n=9$  animals,  
477 Mean: 1.3, 1.4, 1.2, SD: 0.3, 1.1, 0.5 Hz for NT). Data are presented as mean values +/- SEM.

478

479

480 **References**

- 481 1. Lebedev, M.A. & Nicolelis, M.A. Brain-Machine Interfaces: From Basic Science to  
482 Neuroprostheses and Neurorehabilitation. *Physiol Rev* **97**, 767-837 (2017).
- 483 2. Lewis, P.M., Ackland, H.M., Lowery, A.J. & Rosenfeld, J.V. Restoration of vision in  
484 blind individuals using bionic devices: a review with a focus on cortical visual  
485 prostheses. *Brain Res* **1595**, 51-73 (2015).
- 486 3. VanRullen, R. Perceptual Cycles. *Trends Cogn Sci* **20**, 723-735 (2016).
- 487 4. Fernandez, E. et al. Visual percepts evoked with an intracortical 96-channel  
488 microelectrode array inserted in human occipital cortex. *J Clin Invest* **131** (2021).
- 489 5. Beauchamp, M.S. et al. Dynamic Stimulation of Visual Cortex Produces Form Vision in  
490 Sighted and Blind Humans. *Cell* **181**, 774-783 e775 (2020).
- 491 6. Sahel, J.A. et al. Partial recovery of visual function in a blind patient after optogenetic  
492 therapy. *Nat Med* (2021).
- 493 7. Jazayeri, M., Lindbloom-Brown, Z. & Horwitz, G.D. Saccadic eye movements evoked  
494 by optogenetic activation of primate V1. *Nat Neurosci* **15**, 1368-1370 (2012).
- 495 8. Ju, N., Jiang, R., Macknik, S.L., Martinez-Conde, S. & Tang, S. Long-term all-optical  
496 interrogation of cortical neurons in awake-behaving nonhuman primates. *PLoS Biol*  
497 **16**, e2005839 (2018).
- 498 9. Chernov, M.M., Friedman, R.M., Chen, G., Stoner, G.R. & Roe, A.W. Functionally  
499 specific optogenetic modulation in primate visual cortex. *Proc Natl Acad Sci U S A*  
500 **115**, 10505-10510 (2018).
- 501 10. McAlinden, N. et al. Multisite microLED optrode array for neural interfacing.  
502 *Neurophotonics* **6**, 035010 (2019).
- 503 11. Legon, W. et al. Transcranial focused ultrasound modulates the activity of primary  
504 somatosensory cortex in humans. *Nat Neurosci* **17**, 322-329 (2014).
- 505 12. Tufail, Y. et al. Transcranial pulsed ultrasound stimulates intact brain circuits. *Neuron*  
506 **66**, 681-694 (2010).
- 507 13. Deffieux, T. et al. Low-intensity focused ultrasound modulates monkey visuomotor  
508 behavior. *Curr Biol* **23**, 2430-2433 (2013).
- 509 14. Lee, W. et al. Image-Guided Focused Ultrasound-Mediated Regional Brain  
510 Stimulation in Sheep. *Ultrasound Med Biol* **42**, 459-470 (2016).
- 511 15. Tufail, Y., Yoshihiro, A., Pati, S., Li, M.M. & Tyler, W.J. Ultrasonic neuromodulation by  
512 brain stimulation with transcranial ultrasound. *Nat Protoc* **6**, 1453-1470 (2011).
- 513 16. Legon, W., Bansal, P., Tyshynsky, R., Ai, L. & Mueller, J.K. Transcranial focused  
514 ultrasound neuromodulation of the human primary motor cortex. *Sci Rep* **8**, 10007  
515 (2018).
- 516 17. Mehic, E. et al. Increased anatomical specificity of neuromodulation via modulated  
517 focused ultrasound. *PLoS One* **9**, e86939 (2014).
- 518 18. Kim, S. et al. Transcranial focused ultrasound stimulation with high spatial resolution.  
519 *Brain Stimul* **14**, 290-300 (2021).
- 520 19. Cheng, Z. et al. High resolution ultrasonic neural modulation observed via in vivo two-  
521 photon calcium imaging. *Brain Stimul* **15**, 190-196 (2022).
- 522 20. Ye, P.P., Brown, J.R. & Pauly, K.B. Frequency Dependence of Ultrasound  
523 Neurostimulation in the Mouse Brain. *Ultrasound Med Biol* **42**, 1512-1530 (2016).

- 524 21. Constans, C., Mateo, P., Tanter, M. & Aubry, J.F. Potential impact of thermal effects  
525 during ultrasonic neurostimulation: retrospective numerical estimation of  
526 temperature elevation in seven rodent setups. *Phys Med Biol* **63**, 025003 (2018).
- 527 22. Yang, Y. et al. Sonogenetics for noninvasive and cellular-level neuromodulation in  
528 rodent brain. *bioRxiv* <https://doi.org/10.1101/2020.01.28.919910> (2020).
- 529 23. Qiu, Z. et al. Targeted Neurostimulation in Mouse Brains with Non-invasive  
530 Ultrasound. *Cell Rep* **32**, 108033 (2020).
- 531 24. Huang, Y.S. et al. Sonogenetic Modulation of Cellular Activities Using an Engineered  
532 Auditory-Sensing Protein. *Nano Lett* **20**, 1089-1100 (2020).
- 533 25. Wu, X. et al. Sono-optogenetics facilitated by a circulation-delivered rechargeable  
534 light source for minimally invasive optogenetics. *Proc Natl Acad Sci U S A* (2019).
- 535 26. Yang, Y. et al. Sonothermogenetics for noninvasive and cell-type specific deep brain  
536 neuromodulation. *Brain Stimul* **14**, 790-800 (2021).
- 537 27. Ye, J. et al. Ultrasonic Control of Neural Activity through Activation of the  
538 Mechanosensitive Channel Mscl. *Nano Lett* **18**, 4148-4155 (2018).
- 539 28. Soloperto, A. et al. Mechano-sensitization of mammalian neuronal networks through  
540 expression of the bacterial large-conductance mechanosensitive ion channel. *J Cell*  
541 *Sci* **131** (2018).
- 542 29. Sukharev, S.I., Blount, P., Martinac, B., Blattner, F.R. & Kung, C. A large-conductance  
543 mechanosensitive channel in *E. coli* encoded by mscl alone. *Nature* **368**, 265-268  
544 (1994).
- 545 30. Dalkara, D. et al. In vivo-directed evolution of a new adeno-associated virus for  
546 therapeutic outer retinal gene delivery from the vitreous. *Sci Transl Med* **5**, 189ra176  
547 (2013).
- 548 31. Chaffiol, A. et al. A New Promoter Allows Optogenetic Vision Restoration with  
549 Enhanced Sensitivity in Macaque Retina. *Mol Ther* **25**, 2546-2560 (2017).
- 550 32. Verschueren, A. et al. Planar polarity in primate cone photoreceptors: a potential role  
551 in Stiles Crawford effect phototropism. *Commun Biol* **5**, 89 (2022).
- 552 33. Sato, T., Shapiro, M.G. & Tsao, D.Y. Ultrasonic Neuromodulation Causes Widespread  
553 Cortical Activation via an Indirect Auditory Mechanism. *Neuron* **98**, 1031-1041 e1035  
554 (2018).
- 555 34. Guo, H. et al. Ultrasound Produces Extensive Brain Activation via a Cochlear Pathway.  
556 *Neuron* **98**, 1020-1030 e1024 (2018).
- 557 35. Nelidova, D. et al. Restoring light sensitivity using tunable near-infrared sensors.  
558 *Science* **368**, 1108-1113 (2020).
- 559 36. ter Haar, G. Ultrasound bioeffects and safety. *Proc Inst Mech Eng H* **224**, 363-373  
560 (2010).
- 561 37. Sapareto, S.A. & Dewey, W.C. Thermal dose determination in cancer therapy. *Int J*  
562 *Radiat Oncol Biol Phys* **10**, 787-800 (1984).
- 563 38. Aravanis, A.M. et al. An optical neural interface: in vivo control of rodent motor  
564 cortex with integrated fiberoptic and optogenetic technology. *J Neural Eng* **4**, S143-  
565 156 (2007).
- 566 39. Klapoetke, N.C. et al. Independent optical excitation of distinct neural populations.  
567 *Nat Methods* **11**, 338-346 (2014).
- 568 40. Chen, R. et al. Deep brain optogenetics without intracranial surgery. *Nat Biotechnol*  
569 **39**, 161-164 (2021).

- 570 41. Daich Varela, M., Cabral de Guimaraes, T.A., Georgiou, M. & Michaelides, M. Leber  
571 congenital amaurosis/early-onset severe retinal dystrophy: current management and  
572 clinical trials. *Br J Ophthalmol* **106**, 445-451 (2022).
- 573 42. Flores, A.R. et al. Safety, Feasibility, and Patient-Rated Outcome of Sonolucent  
574 Cranioplasty in Extracranial-Intracranial Bypass Surgery to Allow for Transcranioplasty  
575 Ultrasound Assessment. *World Neurosurg* **144**, e277-e284 (2020).
- 576 43. Greenberg, K.P., Pham, A. & Werblin, F.S. Differential targeting of optical  
577 neuromodulators to ganglion cell soma and dendrites allows dynamic control of  
578 center-surround antagonism. *Neuron* **69**, 713-720 (2011).
- 579 44. Lorach, H. et al. Artificial retina : The multichannel processing of the mammalian  
580 retina achieved with a neuromorphic asynchronous light acquisition device. *J Neural*  
581 *Eng* **9**, 066004 (2012).
- 582 45. Kartha, A. et al. Prosthetic Visual Performance Using a Disparity-Based Distance-  
583 Filtering System. *Transl Vis Sci Technol* **9**, 27 (2020).
- 584 46. Montezuma, S.R. et al. Improved localisation and discrimination of heat emitting  
585 household objects with the artificial vision therapy system by integration with  
586 thermal sensor. *Br J Ophthalmol* **104**, 1730-1734 (2020).
- 587
- 588

589 **Methods**

590 **Animals**

591 Experiments were conducted in accordance with the National Institutes of Health Guide for  
592 the Care and Use of Laboratory Animals. Protocols were approved by the Local Animal Ethics  
593 Committee (Committee Charles Darwin no. 5, registration number 9529 and 26889) and  
594 conducted in agreement with Directive 2010/63/EU of the European Parliament. Long Evans  
595 male rats aged between 2 and 12 months and wild-type male mice (C57BL/6J) aged 9 weeks  
596 were obtained from Janvier Laboratories, P23H (line 1) male transgenic rats (9-22 months)  
597 were raised locally.

598

599 **Plasmid cloning & AAV production**

600 Plasmids containing the *Escherichia coli* *mscL* sequence in the WT form and with the G22S  
601 mutation were obtained from Francesco Difato (Addgene plasmids #107454 and #107455)<sup>28</sup>.  
602 To target retinal ganglion cells, the SNCG promoter<sup>31</sup> was inserted into an AAV backbone  
603 plasmid containing the *mscL* sequence fused to the tdTomato gene and the Kir2.1 ER export  
604 signal, to drive expression at the plasma membrane. An AAV2.7m8 vector was used for intra-  
605 vitreous delivery. For targeting neurons in V1 cortical layers, the SNCG promoter was replaced  
606 by the CamKII promoter and an AAV9.7m8 vector was chosen. Recombinant AAVs were  
607 produced by the plasmid cotransfection method, and the resulting lysates were purified by  
608 iodixanol purification<sup>31</sup>.

609

610 **US stimulus**

611 Three focused ultrasound transducers with different central frequencies were used: 0.5 MHz  
612 (diameter  $\varnothing$  = 1 inch = 25.4mm, focal distance  $f$  = 1.25 inch = 31.7 mm) (V301-SU, Olympus),  
613 2.25 MHz ( $\varnothing$  = 0.5 inch = 12.7 mm,  $f$  = 1 inch = 25.4 mm) (V306-SU, Olympus) and 15 MHz ( $\varnothing$   
614 = 0.5 inch = 12.7 mm,  $f$  = 1 inch = 25.4 mm) (V319-SU, Olympus), corresponding to numerical  
615 apertures  $F/\varnothing$ = 1,25 and 2. Acoustic fields radiated by those three focused transducers are  
616 presented in Figure 1 (simulations) and extended figure E3 (experimental measurements). A  
617 TiePie Handyscope (HS5, TiePie Engineering) was used to produce the stimulus waveform,  
618 which was then passed through an 80 dB RF power amplifier (VBA 230-80, Vectawave)  
619 connected to the transducer. Transducer pressure outputs (pressure at focus, 3D pressure

620 maps) were measured in a degassed water tank with a Royer-Dieulesaint heterodyne  
621 interferometer<sup>47</sup>. US stimuli used for *ex vivo* and *in vivo* stimulation had the following  
622 characteristics: 1 kHz pulse repetition frequency with a 50% duty cycle, sonication duration  
623 between 10 and 200 ms and inter-stimulus interval between 0.01 and 2 s. Peak acoustic  
624 pressures were ranging from 0.11-0.88 MPa, 0.3-1.6 MPa, 0.2-1.27 MPa, for the 0.5, 2.25 and  
625 15 MHz transducers, respectively. The corresponding estimated Isppa values were 0.39-25.14  
626 W/cm<sup>2</sup>, 2.92-83.12 W/cm<sup>2</sup> and 1.30-52.37 W/cm<sup>2</sup>.

627

### 628 **Intra-vitreous gene delivery and retinal imaging**

629 Rats were anesthetized<sup>48</sup> and AAV suspension (2  $\mu$ l), containing between 8 and 14 x 10<sup>10</sup> viral  
630 particles, was injected into the center of the vitreous cavity. One month later, tdTomato  
631 fluorescence imaging was performed on the injected eyes, with a Micron IV retinal imaging  
632 microscope (Phoenix Research Laboratories) and Micron Discover V2.2.

633

### 634 **MEA recordings**

635 Retinal pieces were flattened on a filter membrane (Whatman, GE Healthcare Life Sciences)  
636 and placed on a poly-L-lysine (0.1%, Sigma) coated multi-electrode array (electrode diameter  
637 30  $\mu$ m, spacing 200  $\mu$ m, MEA256 200/30 iR-ITO, MultiChannel Systems) with RGCs facing the  
638 electrodes<sup>31</sup>. AMPA/kainate glutamate receptor antagonist 6-cyano-7-nitroquinoxaline-2,3-  
639 dione (CNQX, 25  $\mu$ M, Sigma-Aldrich), the NMDA glutamate receptor antagonist [3H]3-(2-  
640 carboxypiperazin-4-yl) propyl-1-phosphonic acid (CPP, 10  $\mu$ M, Sigma- Aldrich) and a selective  
641 group III metabotropic glutamate receptor agonist, L-(+)-2-amino-4-phosphonobutyric acid (L-  
642 AP4, 50  $\mu$ M, Tocris Bioscience), were bath-applied through the perfusion line. Light stimuli  
643 were delivered with a digital micro-mirror display (DMD, Vialux, resolution 1024x768) coupled  
644 to a white LED light source (MNWHL4, Thorlabs) focused on the photoreceptor plane  
645 (irradiance 1  $\mu$ W/cm<sup>2</sup>). US transducers were coupled with a custom-made coupling cone filled  
646 with degassed water, mounted on a motorized stage (PT3/M-Z8, Thorlabs) placed  
647 orthogonally above the retina. The reflected signal of the MEA chip and the retina was  
648 detected with an US-key device (Lecoeur Electronique). The distance between the retina and  
649 the transducer was equal to the focal length of the transducer; this was verified with the flight  
650 time of the reflected signal. From RGC recordings with a 252-channel preamplifier and  
651 MC\_Rack V4.6.2 (MultiChannel Systems), spikes were sorted with SpykingCircus 0.5

652 software<sup>49</sup>. RGC responses were analyzed with custom scripts written in Matlab (MathWorks  
653 2018b) for classification as ON, ON-OFF or OFF, with the response dominance index<sup>50</sup>.  
654 Latencies were calculated as the time between stimulus onset and the maximum of the  
655 derivative of spike density function. Two classes of US-responding cells were identified on the  
656 basis of latency — short and long latency — by fixing a threshold equal to the minimum of the  
657 latency distribution of the responses of non-transfected cells to US (45 ms). We determined  
658 the peak value A of spike density function for the calculation of response duration, which was  
659 defined as the time interval between the two time points for which the SDF was equal to  $A/e$   
660 ( $e$ : Euler's number). The Fano factor, quantifying spike-count variability, was calculated as  
661 the ratio of the variance of the spike-count to the mean. The Euclidean distance between two  
662 activated cells was weighted according to the maximum firing rate of the cells. The ratio of  
663 the number of activated cells to the size of the area stimulated on the MEA chip was calculated  
664 considering the size of the US focal spot for 2.25 and 15 MHz and the size of the MEA for 0.5  
665 MHz, because the focal spot was larger than the MEA for this frequency. The center of the  
666 response was estimated by weighting the maximum firing rate of each cell by its distance from  
667 other responding cells, and the displacement of the response was calculated as the Euclidean  
668 distance between two center-of-response positions.

669

### 670 **Intracranial injections**

671 AAV suspensions were injected into the right hemisphere at two different locations in rats (2.6  
672 mm ML, 6.8 mm AP and 3.1 mm ML, 7.2 mm AP from bregma) or at one location in mice (2.5  
673 mm ML, 3.5 mm AP from bregma)<sup>48</sup>. For rat injection, the suspension (200 nl, containing  $0.2$ -  
674  $8 \times 10^{15}$  viral particles) was injected at three different depths (1100, 1350 and 1500  $\mu\text{m}$  DV)  
675 with a micro-syringe pump controller (Micro4, World Precision Instruments) operating at a  
676 rate of 50 nl/min and a 10  $\mu\text{l}$  Hamilton syringe. In mice, AAV suspension (1  $\mu\text{l}$  containing  $0.2$ -  
677  $8 \times 10^{15}$  viral particles) was injected at -400  $\mu\text{m}$  DV at a rate of 100 nL/min.

678

### 679 ***In vivo* extracellular recordings**

680 One month after AAV injections, a small craniotomy (5x5 mm square) was drilled above V1 in  
681 the right hemisphere<sup>48</sup>. TdTomato fluorescence was checked with a Micron IV retinal imaging  
682 microscope and Micron Discoverer V2.2 (Phoenix Research Laboratories). A 32-site  $\mu\text{Ecog}$   
683 electrode array (30  $\mu\text{m}$  electrode diameter, 300  $\mu\text{m}$  electrode spacing, FlexMEA36,



684 MultiChannel Systems) was positioned over the transfected region or in a similar zone for  
685 control rats. Multi-electrode (MEA) recordings were performed with a 16-site silicon  
686 microprobe tilted at 45° to the brain surface (electrode diameter 30 μm, spacing 50 μm,  
687 A1x16-5mm-50-703, NeuroNexus Technologies) and MC\_Rack V4.6.2. The MEA was advanced  
688 1100 μm into the cortex with a three-axis micromanipulator (Sutter Instruments, Novato, CA).  
689 US transducers were coupled to the brain with a custom-made coupling cone filled with  
690 degassed water and US gel on a motorized stage. The distance between the cortex and the  
691 transducer was equal to the focal length of the transducer. Visual stimuli were generated by  
692 a white light-collimated LED (MNWHL4, Thorlabs) placed 15 cm away from the eye (4.5  
693 mW/cm<sup>2</sup> at the cornea). Recordings were digitized with 32- and 16-channel amplifiers (model  
694 ME32/16-FAI-μPA, MultiChannel Systems). μEcog recordings were analyzed with custom-  
695 developed Matlab scripts, MEA recordings with SpykingCircus software and custom-  
696 developed Matlab scripts. Response duration was calculated as the interval between the two  
697 time points at which the cortical evoked potential was equal to  $A/e$  (where  $A$  is peak  
698 depolarization and  $e$  is Euler's number). The activated area was defined as the area of the  
699 pseudocolor activation map over which peak depolarization exceeded the background noise  
700 level calculated as 2 times the standard deviation of the signal. The response center was  
701 estimated by weighting the peak depolarization of each electrode by its distance from other  
702 electrodes. Its relative displacement when moving the US transducer, was calculated as the  
703 Euclidean distance of the two positions. For intracortical recordings, cell latency was  
704 estimated as the time between stimulus onset and the maximum of the derivative of spike  
705 density function.

706

### 707 **Surgery for *in vivo* behavioral testing**

708 C57BL6J mice were injected subcutaneously with Buprenorphine (0,05 mg/kg) (Buprécare,  
709 Axience), and Dexamethasone (0,7 mg/kg) (Dexazone, Virbac). Animals were anesthetized  
710 with Isoflurane (5% induction, 2% maintenance, in air/oxygen mixture) and the head was  
711 shaved and cleaned with antiseptic solution. Animals were head-fixed on a stereotactic frame  
712 with an Isoflurane delivering system, eye ointment and a black tissue were applied over the  
713 eyes. Body temperature was maintained at 37°C. After a local injection of Lidocaine (4 mg/kg)  
714 (Laocaine, Centravet), an incision of the skin was made. Two screws were fixed in the skull,  
715 after a small craniotomy (approximately 5 mm x 5 mm) was drilled above V1 in the right

716 hemisphere (0.5 mm steel drill) and cortex buffer was applied. The cortex was covered with a  
717 TPX plastic sheet (125  $\mu\text{m}$  thick) and sealed with dental acrylic cement (Tetric Evoflow). For  
718 behavioral experiments, a metallic headbar (Phenosys) for head fixation was then glued to the  
719 skull on the left hemisphere with dental cement (FUJUCEM II). Animals were placed in a  
720 recovery chamber, with subcutaneous injection of physiological serum and ointment on the  
721 eyes (Ophtalon, Centravet). Buprenorphine was injected during post-surgery monitoring.

722

### 723 **Mouse behavioral tests**

724 Mice were placed on a water restriction schedule until they reached approximately 80-85% of  
725 their weight. Following habituation to the test conditions<sup>35</sup>, mice were trained to respond to a  
726 light stimulus by performing a voluntary detection task: licking a waterspout (blunt 18G  
727 needle, approximately 5 mm from mouth) in response to white light full-field stimulation (200  
728 and 50 ms long) of the left eye (dilated with tropicamide, Mydriaticum Dispersa) 35 trials per  
729 stimulation duration so 70 trials per day. Water ( $\sim 4 \mu\text{L}$ ) was automatically dispensed 500 ms  
730 after the light was switched on, through a calibrated water system. The behavioral protocol  
731 and lick detection were controlled by a custom-made system<sup>35</sup>. The next four days (two-day  
732 break during the weekend), US stimulations were delivered on V1 for 50 ms at three different  
733 pressure values (0.2, 0.7 and 1.2 MPa). These pressure values were delivered in a different  
734 order each day (35 trials each). Inter-trial intervals varied randomly and ranged between 10  
735 and 30 s. The 15 MHz US transducer was coupled to the brain with a custom-made coupling  
736 cone filled with water and US gel. The success rate was calculated by counting the number of  
737 trials in which mice performed anticipatory licks (between stimulus onset and the opening of  
738 the water valve). The session anticipatory lick rate shown in Fig. 6e was calculated by  
739 subtraction from the anticipatory lick rate of a trial, the spontaneous lick rate (calculated on  
740 all the 1 s time windows before each individual stimulus onset (see figure 6a) for all trials) and  
741 multiplication by the success rate. Lick latency was calculated by determining the time to the  
742 first anticipatory lick after stimulus onset. Mice retained for analysis presented a success rate  
743 superior or equal to 60% on the 4<sup>th</sup> day following light stimulation (LS). Then, Light or US  
744 sessions showing a compulsive licking behaviour were excluded based on the outlier  
745 identification made using ROUT method (Q = 1%) on the session spontaneous lick rate  
746 averaging the measurements on all the trials of the session in the 1s time window before the  
747 stimulus onset of the trial.

748

#### 749 **Immunohistochemistry and confocal imaging**

750 Samples were incubated overnight at 4 °C with a monoclonal anti-RBPMS antibody (1:500,  
751 Rabbit, ABN1362, Merck Millipore) for the retina<sup>31</sup>, with a monoclonal anti-NeuN antibody  
752 (1:500; Mouse, clone A60, MAB377, Merck Millipore) for brain sections<sup>48</sup>. The sections were  
753 then incubated with secondary antibodies conjugated with Alexa Fluor 488 (1:500; Donkey  
754 anti-Mouse and Donkey anti-Rabbit IgG 488, polyclonal, A-21202 and A-21206, Invitrogen) and  
755 DAPI (1:1000, D9542, Merck Millipore) for 1 h at room temperature. An Olympus FV1000  
756 confocal microscope with 20x objective (UPLSAPO 20XO, NA: 0.85) was used to acquire images  
757 of flat-mounted retinas and brain sections (Software FV10-ASW V04.02).

758 On confocal images processed with FIJI (ImageJ 1.53q), RBPMS- and NeuN-positive cells were  
759 counted automatically with the *Analyze particles* FIJI plugin. Cells were counted manually by  
760 two different users, with the CellCounter FIJI plugin. Quantification was performed by  
761 acquiring confocal stacks in at least four randomly chosen transfected regions of 0.4 mm<sup>2</sup> (Fig.  
762 E1). For V1 neurons, the sagittal brain slice with the largest tdTomato fluorescence zone was  
763 selected for each animal. A ROI in V1 was manually defined and quantifications were  
764 performed in at least six randomly chosen regions of 0.4 mm<sup>2</sup>.

765

#### 766 **US-induced tissue-heating simulations**

767 A three-fold process was used for the estimation of thermal effects: 1) simulation of the  
768 acoustic fields generated by the three transducers, with realistic acoustic parameters, 2)  
769 verification that non-linear acoustics did not play an important role in heat transfer and 3)  
770 realistic simulations of heat transfer and temperature rise induced at the focus by US in a  
771 linear regime for parameters used in this study.

772 For non-linear simulations, we used Matlab's toolbox *kWave*, by defining the geometry of the  
773 transducer in 3D, and using the following parameters for the propagation medium (water):  
774 sound speed  $c = 1500 \text{ m s}^{-1}$ , volumetric mass  $\rho = 1000 \text{ kg m}^{-3}$ , non-linearity coefficient  $B/A =$   
775  $5$ , attenuation coefficient  $\alpha = 2.2 \cdot 10^{-3} \text{ dB cm}^{-1} \text{ MHz}^{-y}$ , and frequency power law of the  
776 attenuation coefficient  $y = 2$ <sup>51</sup>. We simulated quasi-monochromatic 3D wave-fields using long  
777 bursts of 50 cycles; this gave us both the maximum pressure field in 3D and the waveform at  
778 the focus. Simulations were calibrated by adjusting the input pressure (excitation of the  
779 simulated transducer) to reach the pressure at the focus measured in the water tank with the

780 real transducers. The FWHM focal spot diameter in the xy plane was 4.36, 1.61 and 0.276 mm,  
781 and the major axis in the xz plane was 32.3, 20.6 and 3.75 mm long for the 0.5, 2.25 and 15  
782 MHz transducers, respectively (Fig. 1b-d). Non-linear effects were evaluated by estimating the  
783 relative harmonic content of the waveform at the focus. In the 15 MHz focus transducer  
784 example in figure 1d, the experimental and simulated signals at the focal spot were compared  
785 and found to be highly concordant (Fig. E4a). Furthermore, the amplitude of the second  
786 harmonic is 19.8 dB below the fundamental (20.9 dB in the simulated case), meaning that if  
787 the fundamental energy is E, the second harmonic has energy E/95 (Fig. E4b). Therefore, we  
788 can reasonably neglect the non-linear effects in the calculations of the thermal effects, as they  
789 account for ~1% of the energy involved. The same conclusions were drawn at 0.5 MHz and 15  
790 MHz. Linear wave propagation approximations considerably decreased the computing cost of  
791 the simulations. Linear propagation simulations were conducted with the *Field II* toolbox in  
792 Matlab<sup>52, 53</sup>, in monochromatic mode, with the same medium properties as *kWave* (water), to  
793 obtain the 3D maximum pressure fields. These maximum pressure fields were used to build a  
794 heating source term  $Q_{US} = \frac{\alpha_{np} p_{max}^2}{\rho_b c_b}$ , where  $\alpha_{np}$  is the absorption coefficient of the brain at  
795 the considered frequency (59.04 Np m<sup>-1</sup> at 15 MHz, calculated from  $\alpha_{brain} = 0.21 \text{ dB cm}^{-1} \text{ MHz}^{-\nu}$   
796  $\nu$  and  $\nu = 1.18$ ), the brain volumetric mass  $\rho_{brain} = 1046 \text{ kg m}^{-3}$ , the brain sound speed  $c_{brain} =$   
797  $1546 \text{ m s}^{-1}$ <sup>61,64</sup>, and  $p_{max}$  is the 3D maximum pressure field. This source term was then used  
798 in the resolution of a Pennes's bioheat equation  $\rho_{brain} C_{brain} \cdot \frac{\partial T}{\partial t} = \text{div}(K_t \cdot \nabla T) -$   
799  $\rho_{blood} C_{blood} P_{blood} (T - T_a) + Q$  in *kWave*, where  $C_{brain}$  is the blood specific heat capacity  
800 (3630 J.kg<sup>-1</sup> °C<sup>-1</sup>),  $K_t$  the brain thermal conductivity (0.51 W.m<sup>-1</sup> °C<sup>-1</sup>),  $\rho_{blood}$  the blood density  
801 1050 kg m<sup>-3</sup>,  $C_{blood}$  the blood specific heat capacity (3617 J.kg<sup>-1</sup> °C<sup>-1</sup>),  $P_{blood}$  the blood  
802 perfusion coefficient (9.7 10<sup>-3</sup> s<sup>-1</sup>),  $T_a$  the arterial temperature (37°C), and  $Q = Q_{US} +$   
803  $\rho_{brain} \cdot \gamma_{brain}$  with  $\gamma_{brain}$  the heat generation of the brain tissue (11.37 W kg<sup>-1</sup>)<sup>54, 55</sup>. The initial  
804 condition for brain temperature was set to  $T_0 = 37 \text{ °C}$ .

805

806 This simulation corresponds to the worst-case scenario regarding the temperature rise given:  
807 1) that the acoustic propagation is simulated in water only (non derated value), with a lower  
808 attenuation coefficient (2.2 10<sup>-3</sup> dB cm MHz<sup>-2</sup>) than the brain (0.59 dB cm MHz<sup>-1.27</sup>), even if a  
809 part of the propagation occurs within the brain.  $p_{max}$  maps are, therefore, overestimated. 2)  
810 thermal absorption is simulated in brain tissue only, with a higher absorption coefficient (0.21

811 dB cm MHz<sup>-1.18</sup>) than water, even if a part of the maximum pressure field is actually located  
812 within the water of the acoustic coupling cone.  $Q_{US}$  is, therefore, slightly overestimated. We  
813 mapped the temperature in three spatial dimensions and time, and looked for the point of  
814 maximal temperature rise (Fig. E4 c-f).

815

### 816 **Statistical analysis**

817 Statistical analyses were carried out with Prism software (Prism 9, GraphPad). Values are  
818 expressed and represented as means  $\pm$  the standard error of the mean (SEM) on figures and  
819 in the text unless specified. Data were analyzed in unpaired Welch's *t*-tests (two-tailed) or an  
820 unpaired multiple *t*-tests with Sidak- Bonferroni correction for multiple comparisons.  
821 Statistical tests are provided in figure legends.

822

### 823 **Data availability**

824 Data supporting the findings of this study are available within the paper and Supplementary  
825 information as well as on FigShare :

826 [https://figshare.com/projects/Ectopic\\_expression\\_of\\_a\\_mechanosensitive\\_channel\\_confers](https://figshare.com/projects/Ectopic_expression_of_a_mechanosensitive_channel_confers_spatiotemporal_resolution_to_ultrasound_stimulations_of_neuronal_circuits_for_visual_restitution/154041)  
827 [\\_spatiotemporal\\_resolution\\_to\\_ultrasound\\_stimulations\\_of\\_neuronal\\_circuits\\_for\\_visual\\_r](https://figshare.com/projects/Ectopic_expression_of_a_mechanosensitive_channel_confers_spatiotemporal_resolution_to_ultrasound_stimulations_of_neuronal_circuits_for_visual_restitution/154041)  
828 [estoration/154041](https://figshare.com/projects/Ectopic_expression_of_a_mechanosensitive_channel_confers_spatiotemporal_resolution_to_ultrasound_stimulations_of_neuronal_circuits_for_visual_restitution/154041).

829 All other data are available from the corresponding author upon reasonable request.

830

### 831 **Code availability**

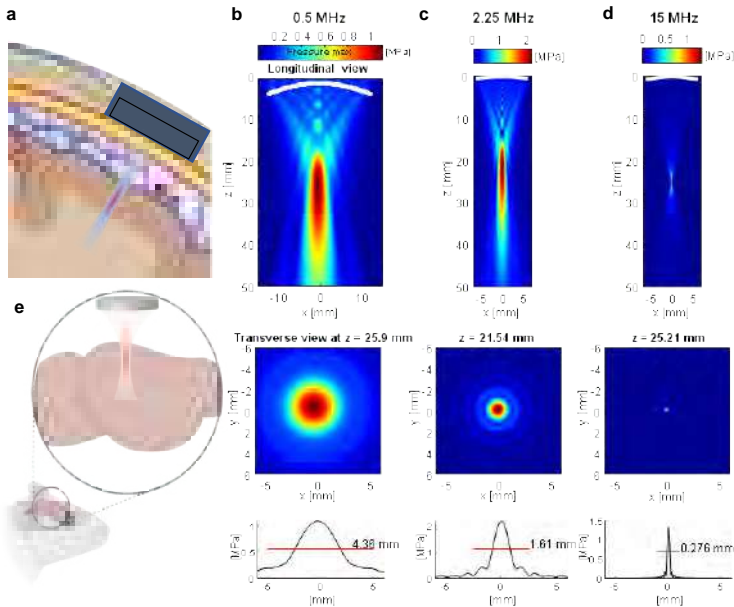
832 The custom Matlab codes are available from the corresponding author upon request.

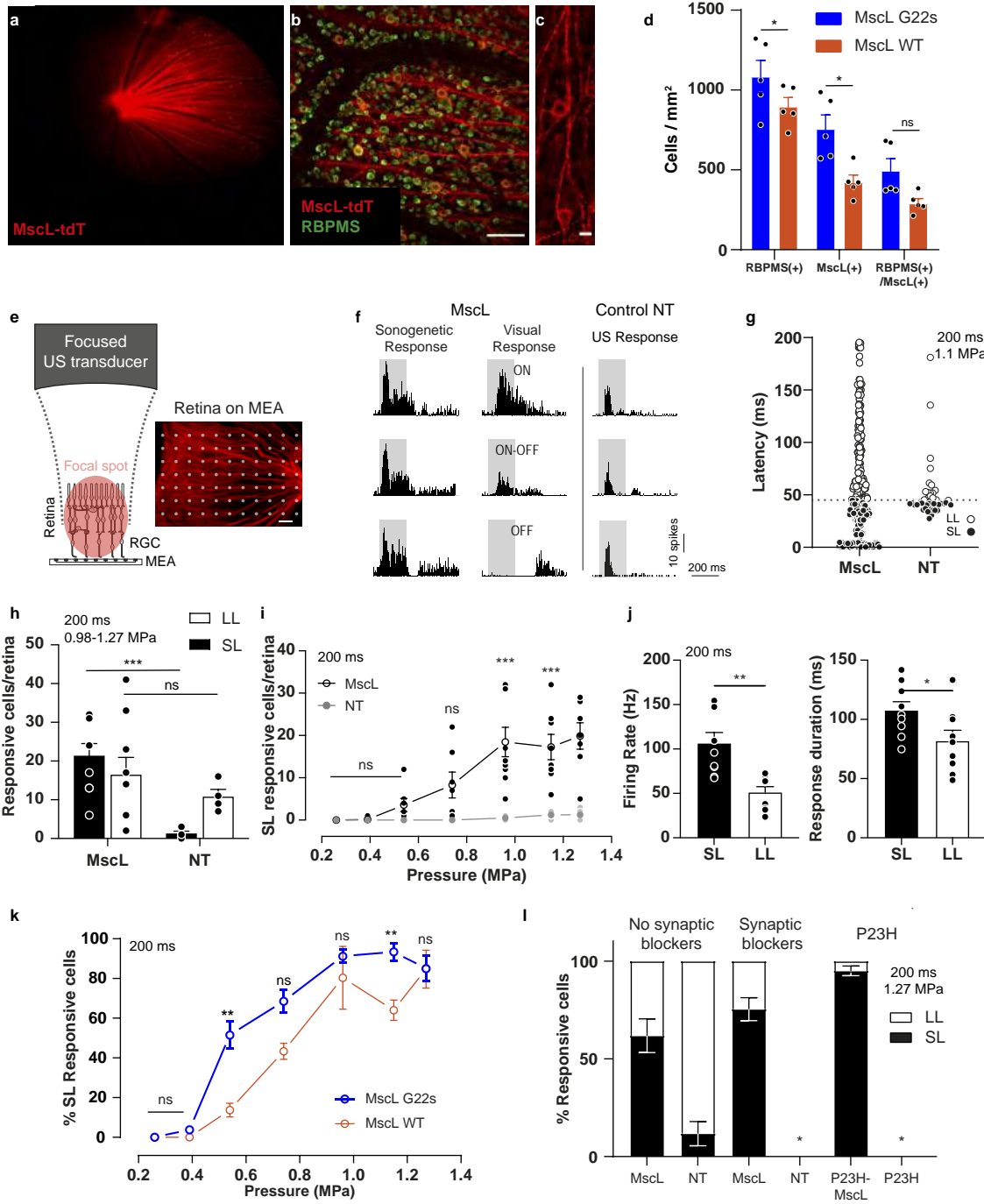
833

### 834 **Methods-only references**

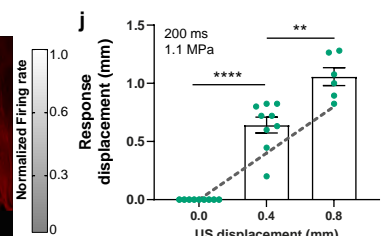
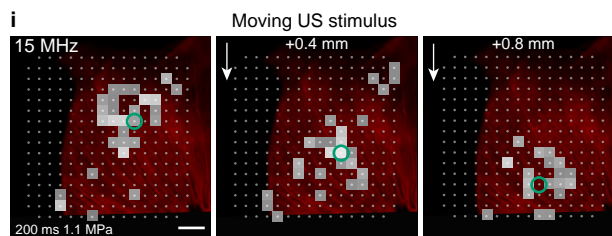
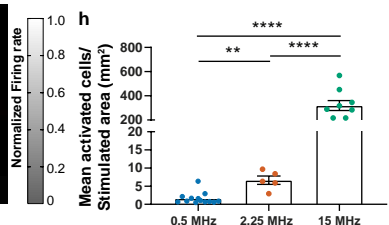
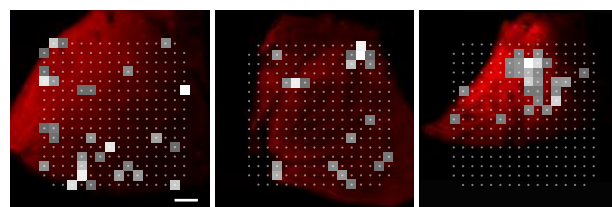
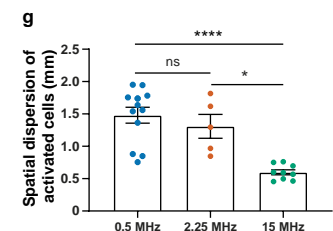
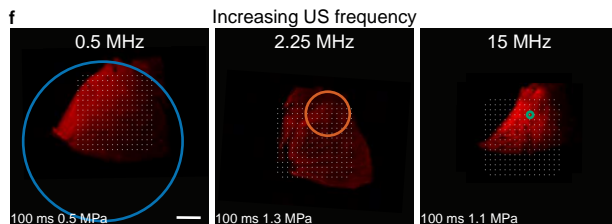
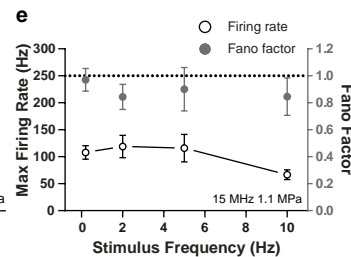
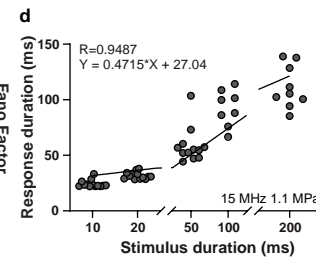
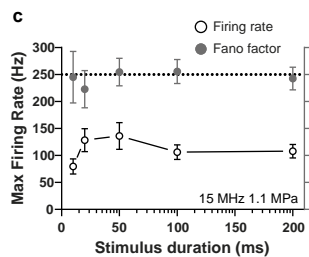
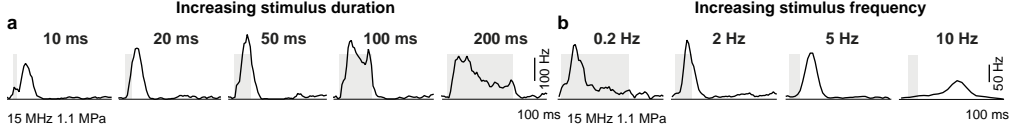
- 835 47. Royer, D. & Dieulesaint, E. Optical probing of the mechanical impulse response of a  
836 transducer. . *Applied Physics Letters* **49**, 1056–1058 (1986).
- 837 48. Provansal, M. et al. Functional ultrasound imaging of the spreading activity following  
838 optogenetic stimulation of the rat visual cortex. *Sci Rep* **11**, 12603 (2021).
- 839 49. Yger, P. et al. A spike sorting toolbox for up to thousands of electrodes validated with  
840 ground truth recordings in vitro and in vivo. *Elife* **7** (2018).
- 841 50. Akerman, C.J., Smyth, D. & Thompson, I.D. Visual experience before eye-opening and  
842 the development of the retinogeniculate pathway. *Neuron* **36**, 869-879 (2002).
- 843 51. Duck, F.A. A. Physical Properties of Tissues: A Comprehensive Reference Network. ,  
844 (Academic Press, ). *Ultrasound in Medicine & Biology* **36**, (Academic Press) (1990).

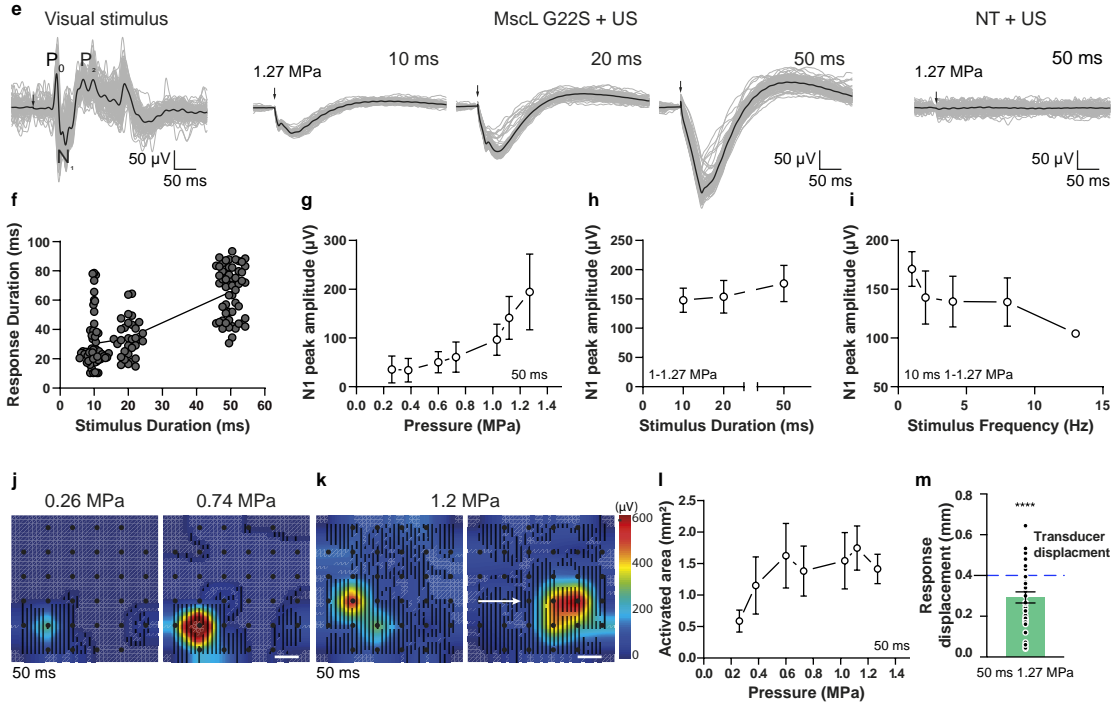
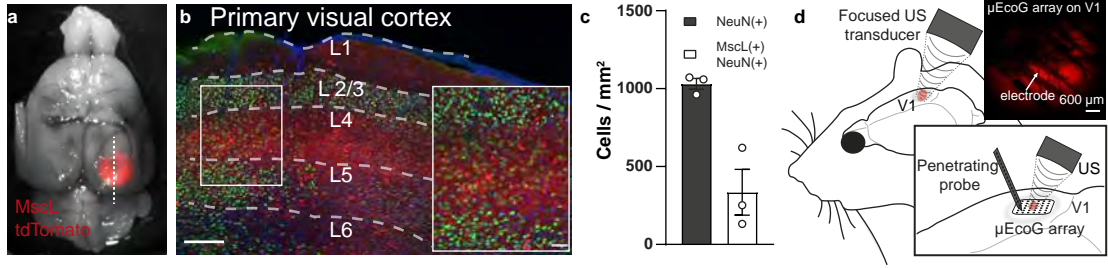
- 845 52. Jensen, J.A. & Svendsen, N.B. Calculation of pressure fields from arbitrarily shaped,  
846 apodized, and excited ultrasound transducers. *IEEE Trans Ultrason Ferroelectr Freq*  
847 *Control* **39**, 262-267 (1992).
- 848 53. Jensen, J.A. A Program for Simulating Ultrasound Systems. *Medical & Biological*  
849 *Engineering & Computing* **34**, 351-353 (1996).
- 850 54. DATABASE., I.F. Available at: [https://itis.swiss/virtual-population/tissue-](https://itis.swiss/virtual-population/tissue-properties/database)  
851 [properties/database](https://itis.swiss/virtual-population/tissue-properties/database). (Accessed: 17th August 2020).
- 852 55. McIntosh, R.L. & Anderson, V.A. A comprehensive tissue properties database  
853 provided for the thermal assessment of a human at rest. *Biophysical Reviews and*  
854 *Letters* **5**, 129–151 (2010).
- 855
- 856

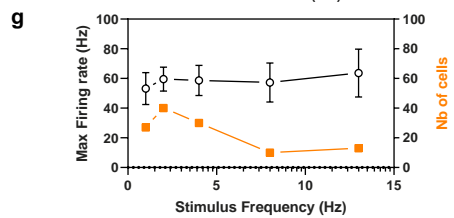
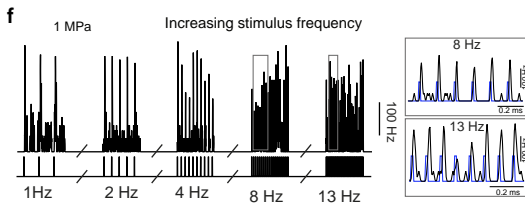
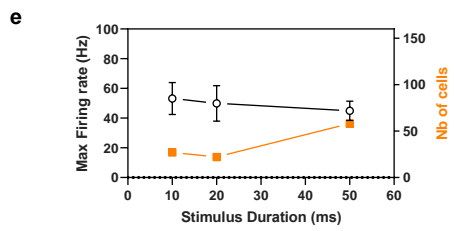
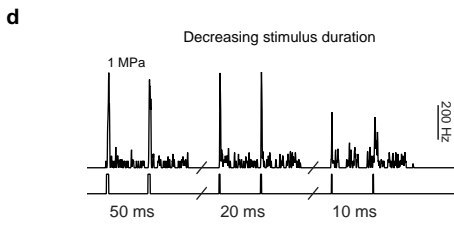
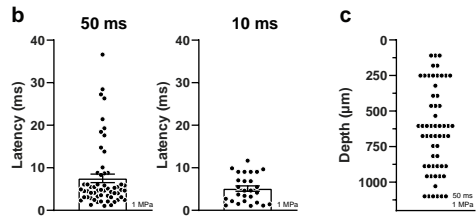
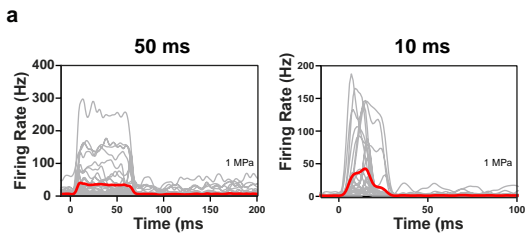


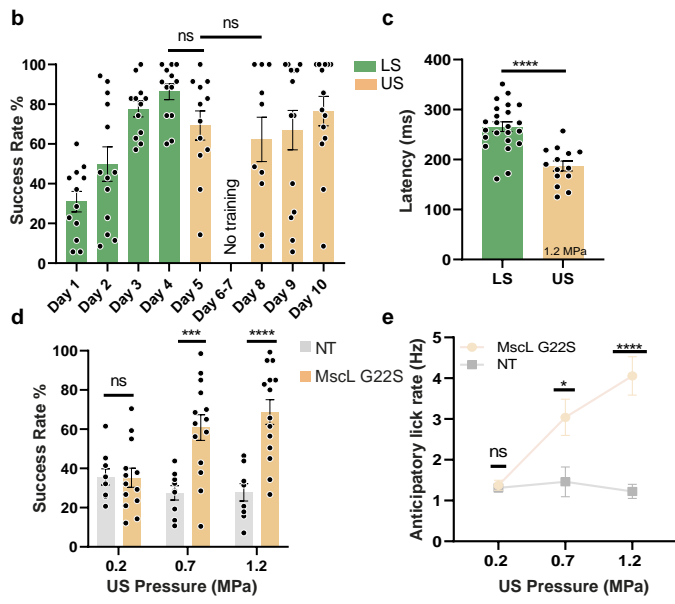
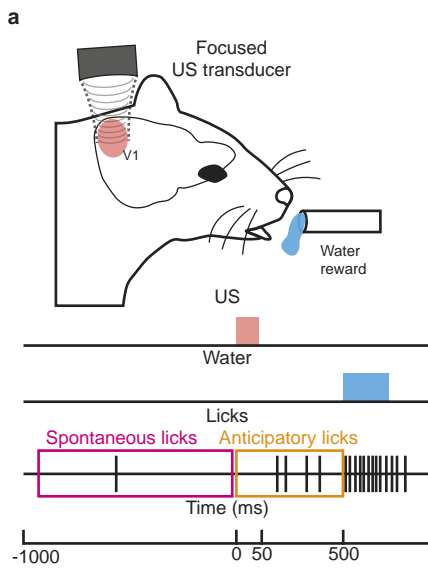












1 **Extended data figures:**

2

3 **Fig. E1 Retinal expression of MscL.** (a) Whole-mount retina expressing MscL WT (red) and labeled with  
4 the RGC-specific anti-RBPMS antibody (green), with DAPI staining of the nucleus (white). Yellow boxes  
5 represent the 8 zones selected for the counting of MscL- and RBPMS-positive cells. (b) Optical section  
6 of a confocal stack showing MscL expression limited to the ganglion cell layer. The scale bars represent  
7 1 mm in (a), 50  $\mu\text{m}$  in (b). Similar results have been obtained for N=10 retinas (5 expressing MscL WT  
8 and 5 expressing MscL G22s).

9

10  
11 **Fig.E2 Retinal sonogenetic response characteristics for US stimuli of different frequencies.** (a) Mean  
12 distribution of the different RGC cell types (ON, OFF, ON-OFF) among short (SL) and long latency (LL)  
13 responses in retinas ( $n=9$ ) expressing MscL (WT and G22s form) following a 15 MHz US stimulus (SD:  
14 21.6, 28.0, 21.8 % for SL, 34.7, 19.4, 30.3 % for LL cells, for ON, ON-OFF and OFF cells respectively). (b)  
15 Mean numbers of RGCs responding to a 15 MHz stimulus of increasing acoustic pressure for MscL WT  
16 ( $n=3$ ), MscL G22s ( $n=5$ ) and NT ( $n=4$ ) retinas (0.39 MPa: \*  $p=0.0163$ ; 0.54 MPa: ns  $p=0.1480$ , \*  
17  $p=0.0168$ ; 0.74 MPa: ns  $p=0.1334$ , \*  $p=0.0312$ ; 0.96 MPa: \*  $p=0.0462$ , \*  $p=0.0279$ ; 1.15 MPa: ns  
18  $p=0.1617$ , \*  $p=0.0145$ ; 1.27 MPa: ns  $p=0.1580$ , \*  $p=0.0144$ ; unpaired two-tailed  $t$  test between MscL  
19 WT and NT in gray and MscL-G22s and NT in blue). (c) Scatter plots and geometric means of RGC  
20 latencies in response to a 15 MHz US stimulus for MscL ( $n=300$  cells SD: 48.8), Blockers+MscL ( $n=57$   
21 cells, SD: 68.0), P23H+MscL ( $n=97$  cells, SD: 37.5), and NT ( $n=41$  cells, SD: 27.4) retinas (\*\*\*\*,  $p=7.3 \cdot 10^{-8}$   
22 for MscL and Blockers MscL vs NT and  $p < .1 \cdot 10^{-15}$  for P23H MscL vs NT, unpaired two-tailed  $t$ -test on  
23 log-transformed values). (d) Cumulative frequency distribution of RGC latencies for MscL,  
24 Blockers+MscL, P23H+MscL, and NT retinas. (e) Mean percentage of cells responding to US stimuli  
25 (normalized against the maximum number of responsive cells in the experiment) of increasing acoustic  
26 pressure for 0.5 MHz (ns  $p=0.1661$ ; \*  $p=0.0292$ ; \*  $p=0.0260$ ; ns  $p=0.8628$ ; ns  $p=0.1316$ ; ns  $p=0.7731$ ;  
27 unpaired  $t$  test), 2.25 MHz (ns  $p=0.1474$ ; ns  $p=0.0522$ ; \*  $p=0.0140$ ; \*\*\*  $p=0.0005$ ; \*\*\*\*  $p < 0.00002$ ; ns  
28  $p=0.5000$ ; unpaired  $t$  test) and 15 MHz US (\*  $p=0.0382$ ; \*\*  $p=0.0065$ ; \*  $p=0.0218$ ; ns  $p=0.8628$ ; ns  
29  $p=0.5859$ ; ns  $p=0.4223$ ; unpaired  $t$  test) US. The lower  $x$  axis represents the corresponding acoustic  
30 intensity ( $I_{\text{spTa}}$ ). (f) Mean response latencies of SL cells for 0.5 and 2.25 MHz ( $n=9$  and 8 retinas). Data  
31 are presented as mean values +/- SEM.

32 **Fig. E3 Experimentally measured US pressure fields.** US pressure fds near the focus for 0.5, 2.25 and  
33 15 MHz focused transducers, measured in water. Color-coded pressure maps in the  $xy$  and  $xz$  planes,  
34 for 0.5, 2.25 and 15 MHz.

35 **Fig. E4 Simulated acoustic fields and temperature increases.** (a) Comparison between a water tank  
36 measurement at the focus with a calibrated hydrophone (black) obtained with the 2.25 MHz  
37 transducer and reaching -1.11 MPa peak negative pressure, and a simulated waveform at the focus  
38 (blue) reaching the same negative pressure. The two waveforms match very well (0.42% error)  
39 ensuring a good match between our simulation setup and physical parameters. (b) Power spectral  
40 density of the measured (black) and simulated (blue) waveforms, showing that simulations can be used  
41 to estimate the importance of non-linear propagation. A second harmonic 20 dB below the  
42 fundamental indicates a factor of 100 in terms of energy, meaning that absorption can be calculated  
43 in a linear approximation. (c-f) Thermal simulations are performed in a two-fold process corresponding  
44 to a worst-case scenario (see methods): propagation in a water medium, and thermal absorption in a  
45 brain-mimicking medium. (h) 3D temperature map at the end of a 200 ms stimulation (at 15 MHz and  
46 1.27 MPa). (d) Temperature rise at the focus for a 15 MHz 200 ms stimulation with the 7 pressures  
47 used in Fig. 1I (0.26, 0.39, 0.54, 0.74, 0.96, 1.15, 1.27 MPa). A zoom on the increasing curve reveals the  
48 fluctuations due to the 1 kHz on-off cycles. (e) Temperature rise at the focus for a 15 MHz 50 ms  
49 stimulation with the same 7 pressures. (f) Temperature rise at the focus for 15 MHz 10ms stimulations  
50 (1 kHz modulation) at a repetition rate of 8 Hz and 13 Hz (used in figure 3o), for focus pressures of 0.96  
51 MPa and 0.54 MPa.

52



53 **Fig. E5 In vivo response displacement to US stimulation.** (a) Relative displacement of the activation  
54 center to the previous position following movement of the US transducer by 0.4 mm in the x and y  
55 direction ( $n=37$  positions on 6 animals). Data are presented as mean values  $\pm$  SEM.

56

57

58 **Fig. E6: MscL G22S expression with the US and light-associative training in mice.** (a) Confocal stack  
59 projection of a sagittal brain slice expressing MscL G22s-tdTomato (red) and labeled with DAPI (blue).  
60 Similar results have been obtained on N=3 animals. (b) Head-fixed and water-restricted mice were  
61 trained for four days to respond to a full-field stimulation of one eye (200 and 50 ms) that preceded a  
62 water reward. Mice responded by licking before (anticipation — successful trial) or after the delivery  
63 of water (failure). The mean success rate increased progressively and mice learned the task (upon 50  
64 ms and 200 ms light stimulation) after four days of training (ns  $p=0.9387$ , two-tailed unpaired  $t$  test,  
65 Mean: 27.9, 45.4, 77.1, 88.8, SD: 17.4, 24.8, 23.6, 10.4% for 200ms, Mean: 30.7, 54.2, 75.9, 88.5, SD:  
66 22.2, 31.0, 17.5, 12.8% for 50ms). (c) Mean rates of successful trials in non-transfected (NT) mice for 4  
67 days of training with light stimulation (50 ms, LS green) and for 4 days of US stimulation (US orange)  
68 (Between Day 4 LS and Day 5 US: 50 ms 1.2 MPa, \*\*\*\*,  $p=0.0000047$ , two-tailed unpaired  $t$  test.  
69 Between Day 5 US and Day 8 US: 50 ms 1.2 MPa, ns,  $p=0.1850$ . Mean: 30.5, 60.3, 73.6, 91.7, 38.1, 23.5,  
70 14.3, 34.0, SD: 28.2, 31.6, 22.1, 10.3, 18.5, 25.5, 21.1, 24.4 %). (d) Pearson correlation scatter plot for  
71 time to first lick after either light (LS) or US stimulation. (e) Identification and exclusion of outlier  
72 sessions (in red) based on the ROUT method, ( $Q = 1\%$ ) for the session spontaneous lick rate measured  
73 on a 1s time window prior to all trials of the session e  $Q_1= 0.9$  Hz, Median = 1.7 Hz,  $Q_3= 2.8$  Hz, Mean=  
74 2.3 Hz, SD= 2.3 Hz. Data are presented as mean values +/- SEM.

